

# INTERNATIONAL STANDARD

**Medical electrical equipment –  
Part 2-16: Particular requirements for basic safety and essential performance of  
haemodialysis, haemodiafiltration and haemofiltration equipment**

IEC 60601-2-16:2008

<https://standards.iteh.ai/en/standards/iec/60601-2-16:2008>

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INTERNATIONAL  
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## INTERNATIONAL ELECTROTECHNICAL COMMISSION

## MEDICAL ELECTRICAL EQUIPMENT –

**Part 2-16: Particular requirements for basic safety and essential performance of haemodialysis, haemodiafiltration and haemofiltration equipment**

## FOREWORD

- 1) The International Electrotechnical Commission (IEC) is a worldwide organization for standardization comprising all national electrotechnical committees (IEC National Committees). The object of IEC is to promote international co-operation on all questions concerning standardization in the electrical and electronic fields. To this end and in addition to other activities, IEC publishes International Standards, Technical Specifications, Technical Reports, Publicly Available Specifications (PAS) and Guides (hereafter referred to as "IEC Publication(s)"). Their preparation is entrusted to technical committees; any IEC National Committee interested in the subject dealt with may participate in this preparatory work. International governmental and non-governmental organizations liaising with the IEC also participate in this preparation. IEC collaborates closely with the International Organization for Standardization (ISO) in accordance with conditions determined by agreement between the two organizations.
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International standard IEC 60601-2-16 has been prepared by IEC subcommittee 62D: Electromedical equipment, of IEC technical committee 62: Electrical equipment in medical practice.

This third edition cancels and replaces the second edition of IEC 60601-2-16, published in 1998. This edition constitutes a technical revision. Changes since the previous edition include, among others, a summary of additional essential performance requirements, revision of terms and definitions, classification of applied parts and limits as numbers for protection against hazardous outputs, in the annex.

The text of this particular standard is based on the following documents:

| FDIS         | Report on voting |
|--------------|------------------|
| 62D/671/FDIS | 62D/681/RVD      |

Full information on the voting for the approval of this particular standard can be found in the report on voting indicated in the above table.

This publication has been drafted in accordance with the ISO/IEC Directives, Part 2.

In this standard, the following print types are used:

- Requirements and definitions: roman type.
- *Test specifications: italic type.*
- Informative material appearing outside of tables, such as notes, examples and references: in smaller type. Normative text of tables is also in a smaller type.
- TERMS DEFINED IN CLAUSE 3 OF THE GENERAL STANDARD, IN THIS PARTICULAR STANDARD OR AS NOTED: SMALL CAPITALS.

In referring to the structure of this standard, the term

- “clause” means one of the seventeen numbered divisions within the table of contents, inclusive of all subdivisions (e.g. Clause 7 includes subclauses 7.1, 7.2, etc.);
- “subclause” means a numbered subdivision of a clause (e.g. 7.1, 7.2 and 7.2.1 are all subclauses of Clause 7).

References to clauses within this standard are preceded by the term “Clause” followed by the clause number. References to subclauses within this particular standard are by number only.

In this standard, the conjunctive “or” is used as an “inclusive or” so a statement is true if any combination of the conditions is true.

The verbal forms used in this standard conform to usage described in Annex H of the ISO/IEC Directives, Part 2. For the purposes of this standard, the auxiliary verb:

- “shall” means that compliance with a requirement or a test is mandatory for compliance with this standard;
- “should” means that compliance with a requirement or a test is recommended but is not mandatory for compliance with this standard;
- “may” is used to describe a permissible way to achieve compliance with a requirement or test.

An asterisk (\*) as the first character of a title or at the beginning of a paragraph or table title indicates that there is guidance or rationale related to that item in Annex AA.

A list of all parts of the IEC 60601 series, published under the general title: *Medical electrical equipment*, can be found on the IEC website.

The committee has decided that the contents of this particular standard will remain unchanged until the maintenance result date indicated on the IEC web site under "<http://webstore.iec.ch>" in the data related to the specific publication. At this date, the publication will be

- reconfirmed;
- withdrawn;
- replaced by a revised edition, or
- amended.

A bilingual version of this publication may be issued at a later date.

The contents of the corrigendum of October 2008 have been included in this copy

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## INTRODUCTION

The minimum safety requirements specified in this particular standard are considered to provide for a practical degree of safety in the operation of HAEMODIALYSIS, HAEMODIAFILTRATION and HAEMOFILTRATION EQUIPMENT.

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## MEDICAL ELECTRICAL EQUIPMENT –

### Part 2-16: Particular requirements for basic safety and essential performance of haemodialysis, haemodiafiltration and haemofiltration equipment

#### 201.1 Scope, object and related standards

Clause 1 of IEC 60601-1:2005 applies, except as follows:

##### 201.1.1 Scope

*Addition:*

This International Standard applies to the BASIC SAFETY and ESSENTIAL PERFORMANCE of HAEMODIALYSIS, HAEMODIAFILTRATION and HAEMOFILTRATION EQUIPMENT, hereafter referred to as HAEMODIALYSIS EQUIPMENT.

This International standard does not take into consideration the DIALYSING FLUID control system of HAEMODIALYSIS EQUIPMENT using regeneration of DIALYSING FLUID and CENTRAL DELIVERY SYSTEMS. It does however take into consideration the specific safety requirements of such HAEMODIALYSIS EQUIPMENT concerning electrical safety and PATIENT safety.

This International standard specifies the minimum safety requirements for HAEMODIALYSIS EQUIPMENT. These devices are intended for use either by medical staff or for use by the PATIENT or other trained personnel under the supervision of medical expertise.

This International standard includes all ME EQUIPMENT that is intended to deliver a HAEMODIALYSIS, HAEMODIAFILTRATION and HAEMOFILTRATION treatment to a PATIENT suffering from kidney failure.

The particular requirements in this International standard do not apply to:

- EXTRACORPOREAL CIRCUITS;
- DIALYSERS;
- DIALYSING FLUID CONCENTRATES;
- water treatment equipment;
- equipment used to perform PERITONEAL DIALYSIS (see IEC 60601-2-39).

If a clause or subclause is specifically intended to be applicable to ME EQUIPMENT only, or to ME SYSTEMS only, the title and content of that clause or subclause will say so. If that is not the case, the clause or subclause applies both to ME EQUIPMENT and to ME SYSTEMS, as relevant.

HAZARDS inherent in the intended physiological function of ME EQUIPMENT or ME SYSTEMS within the scope of this standard are not covered by specific requirements in this standard except in 7.2.13 and 8.4.1 of IEC 60601-1.

NOTE See also 4.2 of IEC 60601-1:2005.

##### 201.1.2 Object

*Replacement:*

The object of this particular standard is to establish BASIC SAFETY and ESSENTIAL PERFORMANCE requirements for HAEMODIALYSIS EQUIPMENT

### 201.1.3 Collateral standards

*Addition:*

This particular standard refers to those applicable collateral standards that are listed in Clause 2 of IEC 60601-1, and Clause 201.2 of this International Standard. (See also Clauses 202, 203, 206, 208, 209 and 210)

IEC 60601-1-3 does not apply.

### 201.1.4 Particular standards

*Replacement:*

In the IEC 60601 series, particular standards may modify, replace or delete requirements contained in IEC 60601-1, *Medical electrical equipment – Part 1: General requirements for basic safety and essential performance*, as appropriate for the particular ME EQUIPMENT under consideration, and may add other BASIC SAFETY and ESSENTIAL PERFORMANCE requirements.

A requirement of a particular standard takes priority over IEC 60601-1.

For brevity, IEC 60601-1 is referred to in this particular standard as the general standard. Collateral standards are referred to by their document number.

The numbering of clauses and subclauses of this particular standard corresponds to that of the general standard with the prefix "201" (e.g. 201.1 in this standard addresses the content of Clause 1 of the general standard) or applicable collateral standard with the prefix "20x" where x is the final digit(s) of the collateral standard document number (e.g. 202.4 in this particular standard addresses the content of Clause 4 of the 60601-1-2 collateral standard, 203.4 in this particular standard addresses the content of Clause 4 of the 60601-1-3 collateral standard, etc.). The changes to the text of the general standard are specified by the use of the following words.

"Replacement" means that the clause or subclause of the general standard or applicable collateral standard is replaced completely by the text of this particular standard.

"Addition" means that the text of this particular standard is additional to the requirements of the general standard or applicable collateral standard.

"Amendment" means that the clause or subclause of the general standard or applicable collateral standard is amended as indicated by the text of this particular standard.

Subclauses or figures which are additional to those of the general standard are numbered starting from 201.101. However due to the fact that definitions in the general standard are numbered 3.1 through 3.139, additional definitions in this standard are numbered beginning from 201.3.201. Additional annexes are lettered AA, BB, etc., and additional items aa), bb), etc.

Subclauses or figures which are additional to those of a collateral standard are numbered starting from 20x, where "x" is the number of the collateral standard, e.g. 202 for IEC 60601-1-2, 203 for IEC 60601-1-3, etc.

The term "this standard" is used to make reference to the general standard, any applicable collateral standards and this particular standard taken together.

Where there is no corresponding, clause or subclause in this particular standard, the, clause or subclause of the general standard or applicable collateral standard, although possibly not relevant, applies without modification; where it is intended that any part of the general standard or applicable collateral standard, although possibly relevant, is not to be applied, a statement to that effect is given in this particular standard.

## 201.2 Normative references

NOTE Informative references are listed in the bibliography beginning on page 52.

Clause 2 of the general standard applies, except as follows:

*Addition:*

IEC 60601-1-9:2007, *Medical electrical equipment – Part 1-9: General requirements for basic safety and essential performance – Collateral Standard: Requirements for environmentally conscious design*

IEC 60601-1-10:2007, *Medical electrical equipment – Part 1-10: General requirements for basic safety and essential performance – Collateral Standard: Requirements for the development of physiologic closed-loop controllers*

IEC 61672-1, *Electroacoustics – Sound level meters – Part 1: Specifications*

ISO 594-2, *Conical fittings with a 6 % (Luer) taper for syringes, needles and certain other medical equipment – Part 2: Lock fittings*

ISO 3744, *Acoustics – Determination of sound power levels of noise sources using sound pressure – Engineering method in an essentially free field over a reflecting plane*

ISO 8638, *Cardiovascular implants and artificial organs – Extracorporeal blood circuit for haemodialysers, haemodiafilters and haemofilters*

## 201.3 Terms and definitions

For the purposes of this document, the terms and definitions given in IEC 60601-1:2005, and IEC 60601-1-10:2007 apply, except as follows:

NOTE An index of defined terms is found beginning on page 53.

### 201.3.8

#### **\*APPLIED PART**

*Replacement:*

EXTRACORPOREAL CIRCUIT and all parts permanently and conductively connected to it (e.g. DIALYSING FLUID circuit)

NOTE See Figure AA.1 in Annex AA.

### 201.3.78

#### **PATIENT CONNECTION**

*Addition:*

NOTE The PATIENT blood lines connectors are the individual points on the APPLIED PART through which current can flow between the PATIENT and the HAEMODIALYSIS EQUIPMENT in NORMAL CONDITION or SINGLE FAULT CONDITION.

*Additions:*

**201.3.201**

**\* HAEMODIALYSIS EQUIPMENT**

ME EQUIPMENT OR ME SYSTEM used to perform HAEMODIALYSIS, HAEMODIAFILTRATION and/or HAEMOFILTRATION

NOTE When the term ME EQUIPMENT is used in headings it is equivalent to HAEMODIALYSIS EQUIPMENT. When the term ME EQUIPMENT is used in the text it is referring to a general ME EQUIPMENT.

**201.3.202**

**HAEMODIALYSIS**

**HD**

process whereby concentrations of water-soluble substances in a PATIENT's blood and an excess of fluid of a PATIENT with renal insufficiency are corrected by bidirectional diffusive transport and ULTRAFILTRATION across a semi-permeable membrane separating the blood from the DIALYSING FLUID

NOTE This process normally includes fluid removal by filtration. This process is usually also accompanied by diffusion of substances from the DIALYSING FLUID into the blood.

**201.3.203**

**HAEMOFILTRATION**

**HF**

process whereby concentrations of water-soluble substances in a PATIENT's blood and an excess of fluid of a PATIENT with renal insufficiency are corrected by unidirectional convective transport via ULTRAFILTRATION across a semi-permeable membrane separating the blood from the DIALYSING FLUID. Ultrafiltrate is simultaneously replaced by an approximately isoosmolar SUBSTITUTION FLUID at a rate such that the difference between the ULTRAFILTRATION rate and the rate of SUBSTITUTION FLUID addition will lead to removal of the excess fluid over the course of the treatment

**201.3.204**

**HAEMODIAFILTRATION**

**HDF**

process whereby concentrations of water-soluble substances in a PATIENT's blood and an excess of fluid of a PATIENT with renal insufficiency are corrected by a simultaneous combination of HD and HF

**201.3.205**

**DIALYSER**

a device containing a semi-permeable membrane that is used to perform HD, HDF or HF

**201.3.206**

**DIALYSING FLUID**

solution intended to exchange solutes and/or water with blood during HD or HDF

NOTE The words "dialysate" and "dialysis fluid" are commonly used as synonyms of DIALYSING FLUID.

**201.3.207**

**DIALYSING FLUID CONCENTRATE**

substances which, when appropriately diluted or dissolved with purified water, produce the DIALYSING FLUID

**201.3.208**

**SUBSTITUTION FLUID**

a fluid administered to the PATIENT via the EXTRACORPOREAL CIRCUIT during HF or HDF

**201.3.209**

**\*ULTRAFILTRATION**

process of fluid removal from the PATIENT'S blood across the DIALYSER

**201.3.210****EXTRACORPOREAL CIRCUIT**

blood lines and any integral ACCESSORY thereof

**201.3.211****TRANSMEMBRANE PRESSURE****TMP**

fluid pressure difference exerted across a semi-permeable membrane

NOTE Generally the mean TMP is used. In practice, the displayed TRANSMEMBRANE PRESSURE is usually estimated from the measured EXTRACORPOREAL CIRCUIT pressure and the measured DIALYSING FLUID pressure, each obtained at a single point.

**201.3.212****\*BLOOD LEAK**

leakage of blood from the blood compartment to the DIALYSING FLUID compartment of the DIALYSER

NOTE When performing an HF process, this involves the filtration fluid section

**201.3.213****ARTERIAL PRESSURE**

pressure measured in the blood withdrawal line of the EXTRACORPOREAL CIRCUIT

NOTE 1 A difference can be made between the pre-pump pressure, which is upstream of the blood pump, and post pump pressure, which is downstream of the blood pump.

**201.3.214****VENOUS PRESSURE**

pressure measured in the blood return line of the EXTRACORPOREAL CIRCUIT

**201.3.215****\*PROTECTIVE SYSTEM**

automatic system, or a constructional feature, specifically designed to protect the PATIENT against HAZARDS which can arise

**201.3.216****\*ONLINE HDF**

HAEMODIAFILTRATION procedure where the HAEMODIALYSIS EQUIPMENT, based on the DIALYSING FLUID, produces the SUBSTITUTION FLUID for the HDF treatment, suitable for injection

**201.3.217****\*ONLINE HF**

HAEMOFILTRATION procedure where the HAEMODIALYSIS EQUIPMENT, based on the DIALYSING FLUID, produces the SUBSTITUTION FLUID for the HF treatment, suitable for injection

**201.3.218****CENTRAL DELIVERY SYSTEM**

Part of a ME SYSTEM which proportions DIALYSING FLUID CONCENTRATE and water for distribution as DIALYSING FLUID to the HAEMODIALYSIS EQUIPMENT or distributes DIALYSING FLUID CONCENTRATE

**201.3.219****NET FLUID REMOVAL**

fluid loss from the PATIENT

NOTE Historically this term was "weight loss".

**201.4 General requirements**

Clause 4 of the general standard applies, except as follows:

**201.4.3 \* ESSENTIAL PERFORMANCE**

*Additional subclauses:*

**201.4.3.101 \* Additional ESSENTIAL PERFORMANCE requirements**

ESSENTIAL PERFORMANCE of HAEMODIALYSIS EQUIPMENT includes, but is not limited to the functions found in the subclauses listed in Table 201.101, which must be met within the tolerances specified by the MANUFACTURER, if applicable:

**Table 201.101 – ESSENTIAL PERFORMANCE requirements**

| Requirement                    | Subclause   |
|--------------------------------|-------------|
| Blood flow                     | 201.4.3.102 |
| DIALYSING FLUID flow           | 201.4.3.103 |
| NET FLUID REMOVAL              | 201.4.3.104 |
| SUBSTITUTION FLUID flow        | 201.4.3.105 |
| Dialysis time                  | 201.4.3.106 |
| DIALYSING FLUID composition    | 201.4.3.107 |
| DIALYSING FLUID temperature    | 201.4.3.108 |
| SUBSTITUTION FLUID temperature | 201.4.3.109 |

NOTE Some ESSENTIAL PERFORMANCES listed in Table 201.101 are dependent on the characteristics of the disposable used (e.g. blood flow is dependent upon the pump segment inner diameter in rotary peristaltic pumps).

**201.4.3.102 Blood flow**

The blood flow for the HAEMODIALYSIS EQUIPMENT shall be as specified by the MANUFACTURER.

NOTE 1 Only a blood flow lower than the set value is considered as negative for the treatment. Therefore the goal of testing is to find the highest negative blood flow error.

*Compliance is checked under the following test conditions for typical peristaltic pumps.*

- Apply a pump segment to the HAEMODIALYSIS EQUIPMENT and let it run for at least 30 min.
- Apply a fluid (e.g. water) with a temperature of 37 °C in the EXTRACORPOREAL CIRCUIT.
- Set the blood flow of the HAEMODIALYSIS EQUIPMENT to 400 ml/min or – if not possible - to the highest possible blood flow.
- Set the ARTERIAL PRESSURE to -200 mmHg.
- Measure the blood flow.

*The values of the measured blood flow shall be within the tolerances specified by the MANUFACTURER in the instructions for use.*

NOTE 2 Pump segment fatigue can reduce the blood flow rate.

NOTE 3 The blood flow rate in peristaltic pumps can be affected by negative input pressures

**201.4.3.103 DIALYSING FLUID flow**

*The DIALYSING FLUID flow for the DIALYSIS EQUIPMENT shall be as specified by the MANUFACTURER.*