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**Breathing system filters for anaesthetic  
and respiratory use —**

**Part 1:  
Salt test method to assess filtration  
performance**

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*Filtres pour matériel d'anesthésie et de réanimation respiratoire —*

*Partie 1: Méthode d'essai saline pour l'évaluation de l'efficacité de  
filtration*

ISO 23328-1:2003

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## Foreword

ISO (the International Organization for Standardization) is a worldwide federation of national standards bodies (ISO member bodies). The work of preparing International Standards is normally carried out through ISO technical committees. Each member body interested in a subject for which a technical committee has been established has the right to be represented on that committee. International organizations, governmental and non-governmental, in liaison with ISO, also take part in the work. ISO collaborates closely with the International Electrotechnical Commission (IEC) on all matters of electrotechnical standardization.

International Standards are drafted in accordance with the rules given in the ISO/IEC Directives, Part 2.

The main task of technical committees is to prepare International Standards. Draft International Standards adopted by the technical committees are circulated to the member bodies for voting. Publication as an International Standard requires approval by at least 75 % of the member bodies casting a vote.

Attention is drawn to the possibility that some of the elements of this document may be the subject of patent rights. ISO shall not be held responsible for identifying any or all such patent rights.

ISO 23328-1 was prepared by Technical Committee ISO/TC 121, *Anaesthetic and respiratory equipment*, Subcommittee SC 3, *Lung ventilators and related equipment*.

ISO 23328 consists of the following parts, under the general title *Breathing system filters for anaesthetic and respiratory use*:

— Part 1: Salt test method to assess filtration performance

— Part 2: Non-filtration aspects

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## Introduction

This part of ISO 23328 gives a method of test for assessing the filtration performance of breathing system filters (BSF).

BSF are used to reduce the number of particulates, including microorganisms, in gases delivered to, and exhaled from, patients.

BSF are exposed to various levels of humidity during clinical use. Exposure of the BSF to humidified air to simulate clinical use forms part of this method (see Annex A), as it is possible that such exposure can influence the filtration performance of the BSF.

In the test, the BSF is challenged with sodium chloride particles of the most penetrating size range, i.e. 0,1  $\mu\text{m}$  to 0,3  $\mu\text{m}$  (see Annex C).

It is recognized that transmission of microorganisms across a filter can occur due to “channeling” and “grow-through”. There are at present no accepted methods to quantify these occurrences. This test method is for comparison purposes only, and has no proven clinical relevance. The results are specific to the test method and no risk factor should be derived from it.

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# Breathing system filters for anaesthetic and respiratory use —

## Part 1: Salt test method to assess filtration performance

### 1 Scope

This part of ISO 23328 gives a short-term airborne sodium chloride particle challenge test method for assessing the filtration performance of breathing system filters (BSF) intended for the filtration of respired gases.

This part of ISO 23328 is applicable to BSF used with a clinical breathing system. It is not applicable to other types of filter, e.g. those designed to protect vacuum sources or gas sample lines, to filter compressed gases, or to protect test equipment for physiological respiratory measurements.

NOTE Non-filtration aspects of BSF are addressed in ISO 23328-2.

### 2 Terms and definitions

For the purposes of this document, the following terms and definitions apply.

#### 2.1

##### **breathing system filter**

##### **BSF**

device intended to reduce transmission of particulates, including microorganisms, in breathing systems

#### 2.2

##### **challenge concentration**

concentration of sodium chloride particles in the airstream as it reaches the BSF

NOTE Challenge concentration is expressed in milligrams per cubic metre.

#### 2.3

##### **penetration concentration**

concentration of sodium chloride particles in the airstream flowing out of the BSF

NOTE Penetration concentration is expressed in milligrams per cubic metre.

#### 2.4

##### **penetration value**

concentration of sodium chloride particles passing through the BSF as a percentage of the concentration in the challenge

#### 2.5

##### **percent filtration efficiency**

100 minus the penetration value

### 3 Method

#### 3.1 Principle

**3.1.1** The ability of a BSF to remove particles is measured by nebulizing a sodium chloride solution into an airstream and passing the sodium chloride particles produced by the nebulizer through the BSF. Annexes B and C give further explanation.

**3.1.2** The generation of aerosols from a nebulizer produces particles that are charged electrostatically. The magnitude of the charge is reduced by mixing the airstream containing the particles with a flow of ionized air so that, when the two flows are mixed, the particles are neutralized to the Boltzmann equilibrium state.

**3.1.3** The flows chosen for testing represent the typical flows likely to be encountered during the intended use of the BSF.

**3.1.4** The performance of the BSF is assessed by measuring the penetration concentration of sodium chloride particles in the airstream leaving the BSF and comparing this with the challenge concentration in the airstream entering the BSF. BSF are tested in the unused state as removed from the packaging and after conditioning to simulate clinical use.

#### 3.2 Test conditions

The ambient conditions during the tests shall be:

- temperature:  $(23 \pm 2) ^\circ\text{C}$ ;
- relative humidity:  $(60 \pm 15) \% \text{ RH}$ ; and
- pressure:  $(96 \pm 10) \text{ kPa}$ .

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#### 3.3 Apparatus

**3.3.1 Flowmeter**, with an accuracy of  $\pm 5 \%$  of the actual value to be measured.

**3.3.2 Sodium chloride aerosol generator<sup>1)</sup>**, capable of generating an aerosol at  $(25 \pm 5) ^\circ\text{C}$  and relative humidity of  $(30 \pm 10) \%$  with a concentration between  $10 \text{ mg}\cdot\text{m}^{-3}$  and  $20 \text{ mg}\cdot\text{m}^{-3}$  which has been neutralized to the Boltzmann equilibrium state.

**3.3.3 Scanning mobility particle sizer<sup>2)</sup>**, or equivalent instrument.

**3.3.4 Suitable forward-light-scattering photometer<sup>3)</sup>**, or equivalent instrument.

#### 3.4 Conditioning of BSF

Condition the BSF in accordance with Annex A.

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1) Model 8118A sodium chloride aerosol generator is an example of a suitable product available commercially from TSI Inc., PO Box 64394, St. Paul, MN 55164, USA. This information is given for the convenience of users of this part of ISO 23328 and does not constitute an endorsement by ISO of this product.

2) Model 3936 scanning mobility particle sizer is an example of a suitable product available commercially from TSI Inc., PO Box 64394, St. Paul, MN 55164, USA. This information is given for the convenience of users of this part of ISO 23328 and does not constitute an endorsement by ISO of this product.

3) Model AFT 8130 forward-light-scattering photometer is an example of a suitable product available commercially from TSI Inc., PO Box 64394, St. Paul, MN 55164, USA. This information is given for the convenience of users of this part of ISO 23328 and does not constitute an endorsement by ISO of this product.



### 3.5 Sample size

It is the responsibility of the BSF manufacturer to document the rationale for the test BSF sample size chosen in order to demonstrate the filtration efficiency of the BSF.

### 3.6 Procedure

NOTE Rationales for various aspects of this method are given in Annex C.

**3.6.1** Set the flowrate through the test apparatus (see Figure 1) to the appropriate value for the intended use of the BSF given in Table 1, using the flowmeter (3.3.1).

**3.6.2** Using the aerosol generator (3.3.2), generate a sodium chloride aerosol at  $(25 \pm 5) ^\circ\text{C}$  and relative humidity of  $(30 \pm 10) \%$ , with a concentration between  $10 \text{ mg}\cdot\text{m}^{-3}$  and  $20 \text{ mg}\cdot\text{m}^{-3}$ , that has been neutralized to the Boltzmann equilibrium state.

**3.6.3** Using the scanning mobility particle sizer (3.3.3), confirm that the sodium chloride test aerosol has a particle size distribution with a count median diameter of  $(0,075 \pm 0,020) \mu\text{m}$  and a geometric standard deviation not exceeding 1,86 at the specified test conditions.

NOTE 1 A particle size distribution with a count median diameter of  $0,075 \mu\text{m}$  and a geometric standard deviation of 1,86 has a mass median aerodynamic diameter (MMAD) of  $0,26 \mu\text{m}$ . See Annex B.

NOTE 2 This is a calibration step of the aerosol generator and only needs to be performed as recommended by the manufacturer.

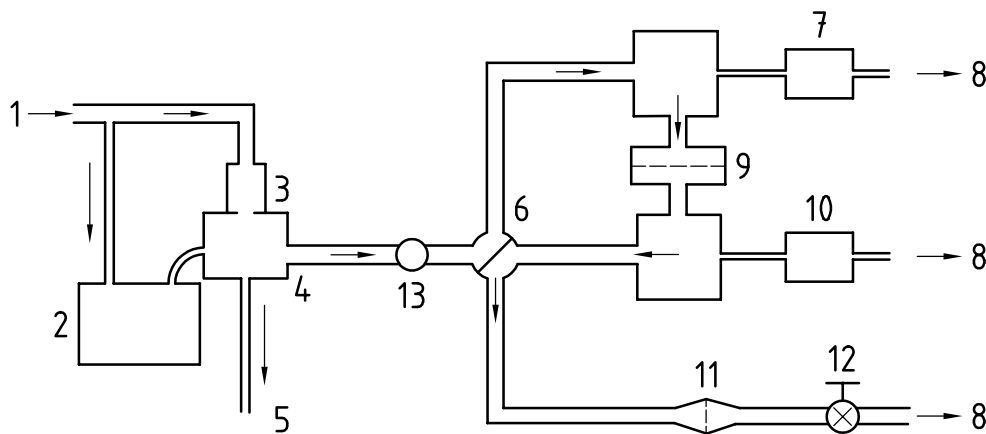
**3.6.4** Without a BSF attached, interconnect the two photometers (3.3.4) and measure the challenge concentration at the upstream photometer. Check that the challenge concentration at the downstream photometer is  $\pm 2,5 \%$  of this value each time the apparatus is switched on, when the airflow is changed and after the BSF sample size (3.5) has been tested.

**3.6.5** Fit a BSF in the unconditioned state to the test apparatus. Test the BSF using the flow direction stated by the manufacturer. If the flow direction is not stated, perform the test with the airstream entering the BSF at the machine port.

**3.6.6** Repeat the generation of aerosol as described in 3.6.2.

**3.6.7** Measure the challenge concentration ( $c_C$ ) and penetration concentration ( $c_P$ ) whilst continuing the test until an aerosol mass of  $(0,2 \pm 0,1) \text{ mg}$  for adult BSF and  $(0,1 \pm 0,05) \text{ mg}$  for paediatric BSF has contacted the BSF.

**3.6.8** Repeat 3.6.5 to 3.6.7 using a BSF in the conditioned state (see 3.4).



Key

- 1

compressed gas
- 2

aerosol generator
- 3

neutralizer
- 4

mixing chamber
- 5

exhaust
- 6

switching valve
- 7

upstream photometer
- 8

to vacuum
- 9

BSF under test
- 10

downstream photometer
- 11

flowmeter
- 12

flow control valve
- 13

location for scanning mobility particle sizer,  
when used; see 3.3.3

Figure 1 — Apparatus for testing BSF

4 Calculation and expression of test results

For the BSF tested, calculate the penetration value (PV) from the following expression:

$$PV = (c_P/c_C) \times 100$$

where

$c_P$  is the penetration concentration, in milligrams per cubic metre, determined in accordance with 3.6;

$c_C$  is the challenge concentration, in milligrams per cubic metre, determined in accordance with 3.6.

Table 1 — Flowrates for testing BSF

BSF intended use	Flowrate l.min <sup>-1</sup>
Paediatric	15
Adult	30

5 Test report

The test report shall include the identification of the BSF, including lot number or date of manufacture and location of manufacturer, the quantity of BSF tested under each condition and the filtration efficiencies of each BSF in the unconditioned and conditioned states.

## Annex A (normative)

### Conditioning of BSF

#### A.1 Principle

BSF are exposed to humidified air in a conditioning apparatus to simulate a period of clinical use before they are tested for filtration efficiency. The conditioning apparatus consists of a humidity-generating patient model connected to a breathing system with or without an inspiratory limb humidity generator. The BSF can be positioned at various points in the breathing system, to simulate clinical use or as recommended by the manufacturer.

#### A.2 Test conditions

The ambient conditions during the conditioning shall be:

- temperature:  $(23 \pm 2) ^\circ\text{C}$ ;
- relative humidity:  $(60 \pm 15) \% \text{ RH}$ ;
- pressure:  $(96 \pm 10) \text{ kPa}$ .

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#### A.3 Apparatus

**A.3.1 Inspiratory limb humidity generator** [see Figure A.1 a)], to increase the temperature and relative humidity of the inspired air if required (see A.4).

**A.3.2 Breathing system** [see Figure A.1 b)], consisting of an inspiratory limb, a Y-piece with a patient connection port, and an expiratory limb, having one-way valves placed at the ends of the breathing system limbs to ensure unidirectional flow through the breathing system.

**A.3.3 Humidity-generating patient model** [see Figure A.1 c)].

The model shall consist of the following:

- a) an insulated chamber, the internal temperature of which is maintained at  $(37 \pm 1) ^\circ\text{C}$ ;
- b) a heated water bath, maintained at  $(37 \pm 1) ^\circ\text{C}$ , through which air is bubbled in both directions;
- c) a rigid reservoir containing a 2 l reservoir bag;
- d) a reciprocating piston/bellows pump.

#### A.4 Positioning of BSF

##### A.4.1 General

The positioning of BSF for conditioning shall be as shown in Figure A.1 and as described in A.4.2 and A.4.3.