
**Dentistry — Compatibility testing —
Part 2:
Ceramic-ceramic systems**

*Médecine bucco-dentaire — Essais de compatibilité —
Partie 2: Systèmes céramo-céramiques*

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ISO copyright office
Ch. de Blandonnet 8 • CP 401
CH-1214 Vernier, Geneva, Switzerland
Tel. +41 22 749 01 11
Fax +41 22 749 09 47
copyright@iso.org
www.iso.org

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Foreword

ISO (the International Organization for Standardization) is a worldwide federation of national standards bodies (ISO member bodies). The work of preparing International Standards is normally carried out through ISO technical committees. Each member body interested in a subject for which a technical committee has been established has the right to be represented on that committee. International organizations, governmental and non-governmental, in liaison with ISO, also take part in the work. ISO collaborates closely with the International Electrotechnical Commission (IEC) on all matters of electrotechnical standardization.

The procedures used to develop this document and those intended for its further maintenance are described in the ISO/IEC Directives, Part 1. In particular the different approval criteria needed for the different types of ISO documents should be noted. This document was drafted in accordance with the editorial rules of the ISO/IEC Directives, Part 2 (see www.iso.org/directives).

Attention is drawn to the possibility that some of the elements of this document may be the subject of patent rights. ISO shall not be held responsible for identifying any or all such patent rights. Details of any patent rights identified during the development of the document will be in the Introduction and/or on the ISO list of patent declarations received (see www.iso.org/patents).

Any trade name used in this document is information given for the convenience of users and does not constitute an endorsement.

For an explanation on the meaning of ISO specific terms and expressions related to conformity assessment, as well as information about ISO's adherence to the WTO principles in the Technical Barriers to Trade (TBT) see the following URL: Foreword - Supplementary information

The committee responsible for this document is ISO/TC 106, *Dentistry*, Subcommittee SC 2, *Prosthetic dental materials*.

This first edition, together with ISO 9693-1, cancels and replaces ISO 9693:1999.

This part of ISO 9693 replaces the bi-material portions of ISO 9693:1999 to focus only on the compatibility of veneering porcelains fired onto substrate ceramics. Tests of all ceramic materials for either metal or ceramic substructures are now contained in a global ceramics standard ISO 6872. Some elements of ISO 9693:1999 remain for all materials (e.g. measurement of thermal expansion coefficients) and one remains only for porcelain fired to zirconia (Schwickerath bond characterization test). New requirements have been added for porcelain-ceramic systems, including thermal shock testing for ceramic-ceramic compatibility (allowing many protocols that are in widespread use within industry).

ISO 9693 consists of the following parts, under the general title *Dentistry — Compatibility testing*:

- *Part 1: Metal-ceramic systems*
- *Part 2: Ceramic-ceramic systems*

Introduction

Dental porcelains and substructure ceramics are suitable for use in fabrication of all-ceramic dental restorations. Their compatibility under mechanical and thermal loading is essential if they are to function in a prosthetic construction. This part of ISO 9693 sets out requirements and test methods for allowing the risks associated with masticatory forces and the oral environment to be assessed.

Specific qualitative and quantitative requirements for freedom from biological hazards are not included in this International Standard, but, in assessing possible biological hazards, reference can be made to ISO 10993-1 and ISO 7405.

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Dentistry — Compatibility testing —

Part 2: Ceramic-ceramic systems

1 Scope

This part of ISO 9693 specifies requirements and test methods to assess the compatibility of ceramic-ceramic materials used for dental restorations by testing composite structures.

The requirements of this part of ISO 9693 apply when different ceramic components are used in combination. Compliance cannot be claimed for either ceramic alone.

For requirements of ceramic materials, see ISO 6872.

2 Normative references

The following documents, in whole or in part, are normatively referenced in this document and are indispensable for its application. For dated references, only the edition cited applies. For undated references, the latest edition of the referenced document (including any amendments) applies.

ISO 1942, *Dentistry — Vocabulary*

ISO 6872:2015, *Dentistry — Ceramic materials*

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3 Terms and definitions

For the purposes of this document, the terms and definitions given in ISO 1942 and ISO 6872 and the following apply.

3.1

ceramic veneer

full structure of fired ceramic layers applied to a substrate material

3.2

conditioning

process of treating the ceramic substructure to enhance the bonding of the veneer ceramic

3.3

liner

substance which, when applied to the ceramic substructure and fired under appropriate time-temperature conditions, may improve aesthetics and/or adherence of ceramic to the coated ceramic surface

4 Requirements

4.1 Biocompatibility

See the Introduction for guidance on biocompatibility.

4.2 Physical properties

4.2.1 General

The individual materials shall fulfil the requirements of ISO 6872 and the thermo-mechanical compatibility tests shall be performed where applicable. The materials shall also comply with the requirements of [4.2.2](#) to [4.2.4](#).

4.2.2 Thermal expansion

The coefficients of thermal expansion of the substructure ceramic and the veneering ceramic shall have been determined according to ISO 6872:2015, 7.4.

It is imperative that the same protocol be used for both the veneering and ceramic substructure (e.g. same lowest temperature).

Test in accordance with [6.1](#).

4.2.3 De-bonding/crack-initiation test (zirconia-porcelain only)

When tested according to [6.3](#), the de-bonding/crack-initiation strength of the zirconia material and at least one specified (named) dental veneering ceramic present shall be greater than 20 MPa. Test in accordance with [6.3](#).

4.2.4 Thermal shock resistance

At least one test for resistance to thermal shock shall be performed according to [6.4.2](#) or [6.4.3](#).

Note The measured values for coefficients of linear thermal expansion are compared with the manufacturer's values as a means of quality control, but the values cannot provide an assurance that the ceramic substructure and ceramic veneer are compatible.

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5 Sampling

5.1 Substructure dental ceramic

The sample shall be adequate to prepare the specimens for testing in accordance with this International Standard. All of the material shall be from the same lot.

5.2 Dental porcelain

Take a sufficient amount of veneering ceramic to carry out the necessary tests in accordance with this International Standard. Perform test with a colour/shade most commonly used. All of the material tested shall be from the same lot.

6 Test methods

6.1 Linear thermal expansion

See ISO 6872:2015, 7.4.

6.2 Glass transition temperature

See ISO 6872:2015, 7.5.

6.3 De-bonding/crack-initiation test (zirconia-porcelain only)

6.3.1 Preparation of test specimens

Prepare six zirconia specimens $(25 \pm 1) \text{ mm} \times (3 \pm 0,1) \text{ mm} \times (0,5 \pm 0,05) \text{ mm}$ in accordance with the manufacturer's procedure for processing the substructures for prostheses. Condition the specimens, observing the manufacturer's instructions. According to the manufacturer's instructions, add dental porcelain to each specimen to form a total ceramic thickness of $(1,1 \pm 0,1) \text{ mm}$ after firing (see [Figure 1](#)). The ceramic layer shall have a rectangular shape and extend the full 3 mm width of the substrate.

If necessary add additional dental porcelain to obtain the required thickness and shape, and fire it. Carefully trim the rectangular shape with a disc. If necessary remove ceramic from the side of the substructure zirconia in order to keep its overall shape.

Submit each specimen to a glaze firing in accordance with the manufacturer's instructions.

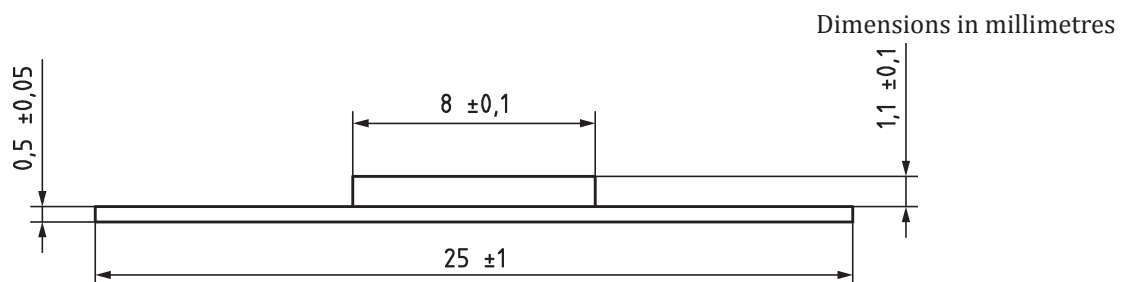


Figure 1 — Test specimen configuration

6.3.2 Determination of fracture force

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6.3.2.1 Apparatus

Flexural-strength testing machine for three-point bending, having a span between supports of 20 mm and capable of a cross-head-speed of $(1,5 \pm 0,5) \text{ mm/min}$. Supports and bending piston shall be rounded to a radius of 1,0 mm.

6.3.2.2 Procedure

The fired specimens are placed in the bending apparatus with the veneering ceramic positioned symmetrically on the side opposite to the applied load. The force is applied at a constant cross-head speed of $(1,5 \pm 0,5) \text{ mm/min}$ and recorded up to failure. The fracture force F_{fail} (in newtons) for each of six specimens is measured for specimens failing by a de-bonding crack occurring at one end of the ceramic layer. Specimens failing by cracks in the middle of the ceramic layer shall be replaced until six appropriate specimens are obtained.

6.3.2.3 Evaluation of de-bonding/crack-initiation strength

6.3.2.3.1 General

The fracture force F_{fail} has to be multiplied with a coefficient k . Coefficient k can be read from [Figure 2](#). The coefficient k is a function of the thickness of the zirconia substrate d_z ($0,5 \pm 0,05$) mm, and the value of Young's modulus E_z of the zirconia substrate.

To read the value k for a certain thickness d_z , first pick the curve for the proper value E_z , then read the value k from the picked curve for the thickness d_z .