



SLOVENSKI STANDARD
oSIST prEN IEC 61846:2023
01-september-2023

Ultrazvok - Terapevtsko usmerjeni viri kratkih tlačnih impulzov - Karakteristike polj

Ultrasonics - Therapeutic focused short pressure pulse sources - Characteristics of fields

Ultraschall - Druckpuls-Lithotripter - Feldcharakterisierung

Ultrasons - Lithotripteurs à ondes de pression - Caractérisation des champs

Ta slovenski standard je istoveten z: prEN IEC 61846:2023

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ICS:

11.040.50	Radiografska oprema	Radiographic equipment
17.140.50	Elektroakustika	Electroacoustics

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SECRETARIAT: United Kingdom	SECRETARY: Mr Petar Luzajic
OF INTEREST TO THE FOLLOWING COMMITTEES:	PROPOSED HORIZONTAL STANDARD: <input type="checkbox"/> Other TC/SCs are requested to indicate their interest, if any, in this CDV to the secretary.
FUNCTIONS CONCERNED: <input type="checkbox"/> EMC <input type="checkbox"/> ENVIRONMENT <input type="checkbox"/> QUALITY ASSURANCE <input type="checkbox"/> SAFETY	
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TITLE:

Ultrasonics – Therapeutic focused short pressure pulse sources – Characteristics of fields

PROPOSED STABILITY DATE: 2027

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INTERNATIONAL ELECTROTECHNICAL COMMISSION

**ULTRASONICS – THERAPEUTIC FOCUSED SHORT PRESSUREPULSE
SOURCES – CHARACTERISTICS OF FIELDS**
FOREWORD

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International Standard IEC 61846 has been prepared by IEC technical committee 87: Ultrasonics.

This second edition cancels and replaces the first edition published in [1998], This edition constitutes a technical revision.

This edition includes the following significant technical changes with respect to the previous edition:

- a) Change of title: Old standard: PRESSURE PULSE LITHOTRIPTERS is changed to "THERAPEUTIC FOCUSED SHORT PRESSURE-PULSE SOURCES" in order to take into account the development in the relevant technical and biomedical applications of such sources, which were originally used only for (kidney) lithotripsy, while recent applications include a wide range for the treatment of e.g. stone diseases, orthopaedic pain, tissue, cardiac and brain diseases. The term "focused" was added to differentiate this standard from IEC 63045 "Non-focusing short pressure pulse sources including ballistic pressure pulse sources" [26].

- 113 The term “short” was added to align the nomenclature to IEC 63045 and differentiate this
114 standard from standards in the HIFU / HITU fields.
- 115 b) Scope and elsewhere in the document: The term “lithotripsy” is changed to “therapy” in
116 order to account for the wide range of applications beyond stone diseases.
- 117 c) 3. Definitions: The “-6 dB” parameter definitions are replaced by “-n dB” to avoid
118 misconceptions in the significance and use of these parameters and to account for newer
119 findings in literature.
120 Additional “n MPa” parameters are introduced for the same reasons.
121 The definitions of “derived” parameters was aligned to those in recently published
122 standards, e.g. IEC 62127-1.
123 New definitions were added which describe parameters appearing in newer relevant
124 literature, e.g. “momentum”, “average positive acoustic pressure”, “cavitation induction
125 index”, “pulse to pulse variability”, “total pressure pulse energy dose”.
- 126 d) 6. Test equipment: The terms “focus hydrophone” and “field hydrophone” were removed to
127 account for newer technical developments. New terms distinguish between “Hydrophones
128 for pressure pulse measurements” and “Hydrophones for quality assurance”
- 129 e) Annexes: Descriptions, tables and figures were edited to account for newer literature and
130 standards as well as technical developments.

131

132 The text of this International Standard is based on the following documents:

FDIS	Report on voting
XX/XX/FDIS	XX/XX/RVD

133

134 Full information on the voting for the approval of this International Standard can be found in the
135 report on voting indicated in the above table.

136 This document has been drafted in accordance with the ISO/IEC Directives, Part 2.

137 The committee has decided that the contents of this document will remain unchanged until the
138 stability date indicated on the IEC website under "http://webstore.iec.ch" in the data related to
139 the specific document. At this date, the document will be

- 140 • reconfirmed,
- 141 • withdrawn,
- 142 • replaced by a revised edition, or
- 143 • amended.

144

145 The National Committees are requested to note that for this document the stability date
146 is 20XX..

147 THIS TEXT IS INCLUDED FOR THE INFORMATION OF THE NATIONAL COMMITTEES AND WILL BE DELETED
148 AT THE PUBLICATION STAGE.

149

150

INTRODUCTION

151 Focused Short Pressure Pulses were initially (since February 1980) applied clinically in
152 lithotripsy, to break up and disrupt calcific deposits within the body, in particular, stones within
153 the renal, biliary and salivary glands tracts. Extracorporeal pressure pulse lithotripsy is up
154 today regarded as the most applied therapeutic option for treating most renal calculi [18], [23],
155 [24].

156 The use of pressure pulses has been evolved to a more general use, often called
157 'Extracorporeal shock wave therapy (ESWT)' which expands its application to a broad range of
158 musculoskeletal conditions, including plantar fasciitis, calcific tendinitis of the shoulder, lateral
159 or medial epicondylitis of the elbow, pain treatment, non-union and delayed union of fractures
160 [25]. Some of these are also treated using unfocused pressure pulse sources, which are
161 specified in another standard (IEC 63045:2020).

162 Several different forms of equipment for lithotripsy and for ESWT are commercially available
163 from a number of manufacturers

164

165 This International Standard specifies methods of measuring and characterizing the acoustic
166 pressure field generated by focusing pressure pulse equipment.

167

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168 **ULTRASONICS – THERAPEUTIC FOCUSED SHORT PRESSURE PULSE**
169 **SOURCES – CHARACTERISTICS OF FIELDS**
170
171

172 **1 Scope**

173 This International Standard is applicable to

- 174 –
175 **therapy equipment** using extracorporeally induced focused pressure pulse waves;
176 – **therapy equipment** producing focused mechanical energy excluding thermal energy.

177 This International Standard does not apply to percutaneous and laser **lithotripsy equipment**.

178 This international standard does not apply to:

- 179 - Histotripsy or other therapeutic ultrasound bursts of longer time duration than that of the
180 **pressure pulse**
181 - Non-focused pressure pulse equipment

182
183 This International Standard specifies

- 184 – measurable parameters which could be used in the declaration of the acoustic output of
185 extracorporeal **focused pressure pulse equipment**,
186 – methods of measurement and characterization of the pressure field generated by **focused**
187 **pressure pulse equipment**.

188 <https://standards.iteh.ai/catalog/standards/sist/dbfa165e-1100-4165-b76c-fa3f16557d9a/osist-pr-en-iec-61846-2023>

189 NOTE – The parameters defined in this International Standard do not – at the present time – allow quantitative
190 statements to be made about effectiveness and possible hazard. In particular, it is not possible to make a statement
191 about the limits for these effects.

192 While this particular standard has been developed for equipment intended for use in **lithotripsy**,
193 it has been developed such that, as long as no other specific standards are available to be used
194 for other medical applications of therapeutic extracorporeal **focused pressure pulse**
195 equipment, this standard may be used as a guideline.

196

197 **2 Normative references**

198 The following documents are referred to in the text in such a way that some or all of their content
199 constitutes requirements of this document. For dated references, only the edition cited applies.
200 For undated references, the latest edition of the referenced document (including any
201 amendments) applies.

202 IEC 60050-13:2011 International Electrotechnical Vocabulary – Part. 113: Physics for
203 electrotechnology,

204 IEC/TR 62781:2012 Ultrasonics – Conditioning water for ultrasonic measurement,

205 IEC 60565-1:2020 Underwater acoustics – Hydrophones – Calibration of hydrophones –
206 Part 1: Procedures for free field calibration of hydrophones,

207 IEC 60565-2:2019 Underwater acoustics – Hydrophones – Calibration of hydrophones – Part 2:
208 Procedures for low frequency pressure calibration,

209 IEC 62127-1:2022 ULTRASONICS – HYDROPHONES – Part 1: Measurement and
210 characterization of medical ultrasonic fields

211 3 Terms and definitions

212 For the purposes of this document, the following terms and definitions apply.

213 ISO and IEC maintain terminological databases for use in standardization at the following
214 addresses:

- 215 • IEC Electropedia: available at <http://www.electropedia.org/>
- 216 • ISO Online browsing platform: available at <http://www.iso.org/obp>

217

218 3.1

219 acoustic pulse energy

220

221 3.1.1

222 derived acoustic pulse energy

223 E_R

224 spatial integral of the **derived pulse-intensity integral** over a circular cross-sectional area of
225 radius R in the x-y plane which contains the **focus**

226 Note 1 to entry: The radius R is derived either from the largest size of a threshold value of pressure, derived pulse
227 intensity integral, or any other quantity. This quantity is stated as a second index. The manufacturer chooses the
228 appropriate quantity and threshold value based on their clinical significance, based on literature and/or risk analysis."

229 Note 2 to entry: The **derived acoustic pulse energy** is expressed in Units of joules (J)

230 3.1.2

231 derived focal acoustic pulse energy

232 E_f

233 spatial integral of the **derived pulse-intensity integral** over the **focal cross-sectional area**

234 Note 1 to entry: The **derived focal acoustic pulse energy** is expressed in Units of joules (J)

235 3.2

236 beam axis

237 line passing through the geometric centre of the aperture of the **pressure pulse** generator and
238 the **focus**

239 Note 1 to entry: This line is taken as the z axis. See 6.1 and clause 7

240 3.3

241 compressional pulse duration

242 $t_{FWHM_{pC}}$

243 time interval beginning at the first time the **instantaneous acoustic pressure** exceeds 50 %
244 of the **peak-compressional acoustic pressure** and ending at the next time the **instantaneous**
245 **acoustic pressure** has that value (see figure C.1)

246 Note to entry: The **compressional pulse duration** is expressed in Units of seconds (s)

247 Note 1 to entry: The subscript "FWHM" stands for "full width, half maximum".

248 3.4

249 rarefactional pulse duration

250 t_{pr}

251 time interval beginning at the first time the **instantaneous acoustic pressure** is less than 10%
252 of the **peak-rarefactional acoustic pressure** after the decay of the **peak-compressional**
253 **acoustic pressure** and ending at the next time the **instantaneous acoustic pressure** has that
254 value (see figure C.1)

255 Note to entry: The **compressional pulse duration** is expressed in Units of seconds (s)

256 **3.5**
 257 **derived pulse-intensity integral**
 258 $PII(x,y,z)$ time integral of the **instantaneous intensity** at a particular point in a **pressure pulse**
 259 field over the **pressure pulse waveform**

260 Note 1 to entry: This parameter is often called "energy flux density".

261 Note 2 to entry: The **derived pulse-intensity integral** is expressed in units of joule per metre squared (J/m^2).

262 Note 3 to entry: The temporal limits for the calculation of the **derived pulse-intensity integral** are specified in the
 263 **temporal integration limits** definitions.

264 **3.6**
 265 **end-of-cable loaded sensitivity of a hydrophone**

266 M_L

267 quotient of the Fourier transformed hydrophone voltage-time signal at the end of any integral
 268 cable or output connector of a **hydrophone** or hydrophone-assembly, when connected to a
 269 specified electric load impedance, to the Fourier transformed **instantaneous acoustic**
 270 **pressure** waveform in the undisturbed free field of a plane wave in the position of the acoustic
 271 centre of the **hydrophone** if the **hydrophone** were removed

272 Note 1 to entry: The **end-of-cable loaded sensitivity of a hydrophone** is a complex-valued parameter. Its modulus
 273 is expressed in units of volt per pascal ($V Pa^{-1}$). Its phase angle is expressed in degrees, and represents the phase
 274 difference between the electrical voltage and the sound pressure.

275 Note 2 to entry: Reformulated from 3.25 of IEC 62127-1:2022.

276

277 **3.7**
 278 **focal $-n$ dB cross-sectional area**

279 $A_{f,n\text{dB}}$

280 area of the **peak-compressional acoustic pressure** contour which is in the plane,
 281 perpendicular to the **beam axis** and containing the **focus**, where all points on the contour have
 282 a pressure of $-n$ dB relative to the value at the **focus**

283 Note 1 to entry: The value of n and the axial distance z from the measurement centre point is stated as subscript.

284 Note 2 to entry: Typical values of $-n$ dB are: -3 dB, -6 dB, -10 dB, -12 dB, -20 dB. Reasonable values of n for
 285 clinical approval and communication to the users can be identified by a risk analysis process, by applicable safety
 286 standards, by consulting notified bodies, expert communities (e.g. ISMST – International Society for Medical
 287 Shockwave Treatment) or through literature.

288 Note 3 to entry: The **focal $-n$ dB cross-sectional area** is expressed in units of metre squared (m^2).

289 **3.8**
 290 **focal $-n$ dB extent**

291 $f_{z,n\text{dB}}$

292 shortest distance along the z axis that connects points on the contour of **peak-compressional**
 293 **acoustic pressure** which have a value of $-n$ dB relative to the acoustic pressure at the **focus**

294 Note 1 to entry: The value of n is stated as subscript.

295 Note 2 to entry: Typical values of $-n$ dB are: -3 dB, -6 dB, -10 dB, -12 dB, -20 dB. Reasonable values of n for
 296 clinical approval and communication to the users can be identified by a risk analysis process, by applicable safety
 297 standards, by consulting notified bodies, expert communities (e.g. ISMST – International Society for Medical
 298 Shockwave Treatment) or through literature.

299 Note 3 to entry: The **focal $-n$ dB extent** is expressed in metres (m).

300 **3.9**
 301 **focal $-n$ dB volume**

302 $V_{f,n\text{dB}}$

303 volume in space contained within the surface defined by the $-n$ dB (relative to the **focal**
 304 **pressure maximum** value) **peak-compressional acoustic pressure** contours measured
 305 around the **focus**

306 Note 1 to entry: It may be difficult to measure $-n$ dB points throughout the volume around the **focus**. It is reasonable
 307 in practice to approximate the **focal $-n$ dB volume** from measurements taken in three orthogonal directions: the
 308 **beam axis** (z axis); the direction of maximum beam diameter (x axis); the axis perpendicular to the x axis (y axis),
 309 which are also orthogonal to the **beam axis**.

310 Note 2 to entry: Typical values of $-n$ dB are: -3 dB, -6 dB, -10 dB, -12 dB, -20 dB. Reasonable values of n for
 311 clinical approval and communication to the users can be identified by a risk analysis process, by applicable safety