



Designation: F543 – 13

# Standard Specification and Test Methods for Metallic Medical Bone Screws<sup>1</sup>

This standard is issued under the fixed designation F543; the number immediately following the designation indicates the year of original adoption or, in the case of revision, the year of last revision. A number in parentheses indicates the year of last reappraisal. A superscript epsilon ( $\epsilon$ ) indicates an editorial change since the last revision or reappraisal.

*This standard has been approved for use by agencies of the Department of Defense.*

## 1. Scope

1.1 This specification provides requirements for materials, finish and marking, care and handling, and the acceptable dimensions and tolerances for metallic bone screws that are implanted into bone. The dimensions and tolerances in this specification are applicable only to metallic bone screws described in this specification.

1.2 This specification provides performance considerations and standard test methods for measuring mechanical properties in torsion of metallic bone screws that are implanted into bone. These test methods may also be applicable to other screws besides those whose dimensions and tolerances are specified here. The following annexes are included:

1.2.1 **Annex A1**—Test Method for Determining the Torsional Properties of Metallic Bone Screws.

1.2.2 **Annex A2**—Test Method for Driving Torque of Medical Bone Screws.

1.2.3 **Annex A3**—Test Method for Determining the Axial Pullout Strength of Medical Bone Screws.

1.2.4 **Annex A4**—Test Method for Determining the Self-Tapping Performance of Self-Tapping Medical Bone Screws.

1.2.5 **Annex A5**—Specifications for Type HA and Type HB Metallic Bone Screws.

1.2.6 **Annex A6**—Specifications for Type HC and Type HD Metallic Bone Screws.

1.2.7 **Annex A7**—Specifications for Metallic Bone Screw Drive Connections.

1.3 This specification is based, in part, upon ISO 5835, ISO 6475, and ISO 9268.

1.4 The values stated in SI units are to be regarded as standard. No other units of measurement are included in this standard.

1.5 Multiple test methods are included in this standard. However, it must be noted that the user is not obligated to test using all of the described methods. Instead, the user should

only select test methods that are appropriate for a particular device design. In most instances, only a subset of the herein described test methods will be required.

1.6 This standard may involve the use of hazardous materials, operations, and equipment. *This standard does not purport to address all of the safety concerns, if any, associated with its use. It is the responsibility of the user of this standard to establish appropriate safety and health practices and determine the applicability of regulatory limitations prior to use.*

## 2. Referenced Documents

2.1 *ASTM Standards*:<sup>2</sup>

- E4 Practices for Force Verification of Testing Machines
- E6 Terminology Relating to Methods of Mechanical Testing
- E8 Test Methods for Tension Testing of Metallic Materials
- E122 Practice for Calculating Sample Size to Estimate, With Specified Precision, the Average for a Characteristic of a Lot or Process
- F67 Specification for Unalloyed Titanium, for Surgical Implant Applications (UNS R50250, UNS R50400, UNS R50550, UNS R50700)
- F86 Practice for Surface Preparation and Marking of Metallic Surgical Implants
- F116 Specification for Medical Screwdriver Bits
- F136 Specification for Wrought Titanium-6Aluminum-4Vanadium ELI (Extra Low Interstitial) Alloy for Surgical Implant Applications (UNS R56401)
- F138 Specification for Wrought 18Chromium-14Nickel-2.5Molybdenum Stainless Steel Bar and Wire for Surgical Implants (UNS S31673)
- F565 Practice for Care and Handling of Orthopedic Implants and Instruments
- F620 Specification for Titanium Alloy Forgings for Surgical Implants in the Alpha Plus Beta Condition
- F799 Specification for Cobalt-28Chromium-6Molybdenum Alloy Forgings for Surgical Implants (UNS R31537, R31538, R31539)

<sup>1</sup> This specification is under the jurisdiction of ASTM Committee F04 on Medical and Surgical Materials and Devices and is the direct responsibility of Subcommittee Osteosynthesis.

Current edition approved May 1, 2013. Published June 2013. Originally approved in 1977. Last previous edition approved in 2009 as F543 – 07<sup>ε1</sup>. DOI: 10.1520/F0543-13.

<sup>2</sup> For referenced ASTM standards, visit the ASTM website, [www.astm.org](http://www.astm.org), or contact ASTM Customer Service at [service@astm.org](mailto:service@astm.org). For *Annual Book of ASTM Standards* volume information, refer to the standard's Document Summary page on the ASTM website.

**F983** Practice for Permanent Marking of Orthopaedic Implant Components

**F1295** Specification for Wrought Titanium-6Aluminum-7Niobium Alloy for Surgical Implant Applications (UNS R56700)

**F1314** Specification for Wrought Nitrogen Strengthened 22 Chromium-13 Nickel-5 Manganese-2.5 Molybdenum Stainless Steel Alloy Bar and Wire for Surgical Implants (UNS S20910)

**F1472** Specification for Wrought Titanium-6Aluminum-4Vanadium Alloy for Surgical Implant Applications (UNS R56400)

**F1537** Specification for Wrought Cobalt-28Chromium-6Molybdenum Alloys for Surgical Implants (UNS R31537, UNS R31538, and UNS R31539)

**F1586** Specification for Wrought Nitrogen Strengthened 21Chromium-10Nickel-3Manganese-2.5Molybdenum Stainless Steel Alloy Bar for Surgical Implants (UNS S31675)

**F1713** Specification for Wrought Titanium-13Niobium-13Zirconium Alloy for Surgical Implant Applications (UNS R58130) (Withdrawn 0)<sup>3</sup>

**F1813** Specification for Wrought Titanium-12Molybdenum-6Zirconium-2Iron Alloy for Surgical Implant (UNS R58120)

**F1839** Specification for Rigid Polyurethane Foam for Use as a Standard Material for Testing Orthopaedic Devices and Instruments

**F2066** Specification for Wrought Titanium-15 Molybdenum Alloy for Surgical Implant Applications (UNS R58150)

## 2.2 ISO Standards:

**5835** Implants for Surgery—Metal Bone Screws with Hexagonal Driver Connection, Spherical Under Surface of Head, Asymmetrical Thread—Dimensions<sup>4</sup>

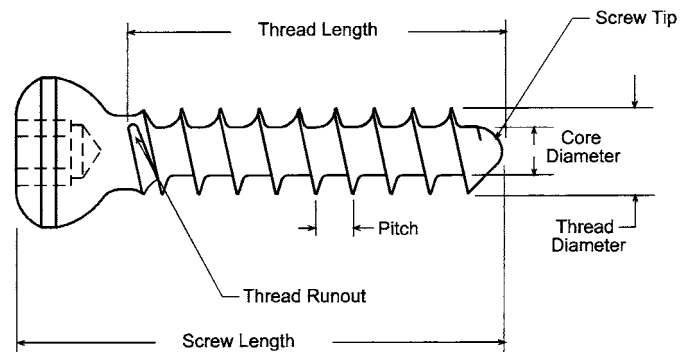
**6475** Implants for Surgery—Metal Bone Screws with Asymmetrical Thread and Spherical Under-Surface—Mechanical Requirements and Test Methods<sup>4</sup>

**8319-1** Orthopaedic Instruments—Drive connections—Part 1: Keys for use with hexagon socket heads<sup>4</sup>

**8319-2** Orthopaedic Instruments—Drive connections—Part 2: Screwdrivers for single slot head screws, screws with cruciate and cross-cessed head screws<sup>4</sup>

**9268** Implants for Surgery—Metal Bone Screws with Conical Under-Surface of Head—Dimensions<sup>4</sup>

**10664** Hexalobular Internal Driving Feature for Bolts and Screws<sup>4</sup>



**FIG. 1** Schematic of Screw Terms

3.1.2 *breaking angle*—angle of rotation when the screw fails in torsion as demonstrated by a rapid decrease in the indicated torque.

3.1.3 *buttress thread*—an asymmetrical thread profile characterized by a pressure flank which is nearly perpendicular to the screw axis.

3.1.4 *cancellous screw*—a screw designed primarily to gain purchase into cancellous bone. Cancellous screws typically have an HB (see 4.1.2) thread and may or may not be fully threaded.

3.1.5 *cortical screw*—a screw designed primarily to gain biocortical purchase into cortical bone. Cortical screws typically have a HA (see 4.1.1) thread and are fully threaded.

3.1.6 *core diameter*—the smallest diameter of the threaded portion of the screw measured at the thread root. This is also known as the minor diameter or root diameter.

3.1.7 *gage length*—the distance between the holding device (for example, a split collet) and the underside of the screw head.

3.1.8 *grip length*—the length of threads held fast in the split collet or other holding mechanism.

3.1.9 *insertion depth*—the threaded length as inserted into the test block.

3.1.10 *insertion torque*—the amount of torque required to overcome the frictional force between the screw and the material used for testing while driving the screw into the material.

3.1.11 *maximum torque* (N·m)—the largest value of torque recorded during the period of rotation before screw failure in torsional shear when tested in accordance with Annex A1.

3.1.12 *nontapping screw*—a screw that has a tip that does not contain a flute. Nontapping screws usually require a tap to be inserted into the pilot hole before the insertion of the screw, when used in moderate or hard bone.

3.1.13 *partially threaded screw*—a screw whose threaded portion does not extend fully from the screw point to the screw head but instead has a smooth shaft running between the head and threads.

3.1.14 *pilot hole*—the hole drilled into the bone into which the screw tip is inserted. The pilot hole is normally slightly larger than the screw's core diameter. However, if the screw is

## 3. Terminology

3.1 *Definitions*—Some of the terms defined in this section are shown in Fig. 1.

3.1.1 *axial pullout strength*—the tensile force required to fail or remove a bone screw from a material into which the screw has been inserted.

<sup>3</sup> The last approved version of this historical standard is referenced on [www.astm.org](http://www.astm.org).

<sup>4</sup> Available from American National Standards Institute, 25 W. 43rd St., 4th Floor, New York, NY 10036.

to be used to provide compression across a fracture, a portion of the pilot hole may be larger to allow for a clearance fit.

3.1.15 *pitch*—the length between the thread crests.

3.1.16 *removal torque*—the amount of torque required to overcome the frictional force between the screw and the material used for testing while removing the screw from the material (for example, counterclockwise rotation for right-hand thread).

3.1.17 *screw head*—the end of the screw which is opposite of the tip and from which the means of inserting the screw is coupled.

3.1.18 *screw length*—the overall length of the screw measured from the screw head to the screw tip.

3.1.19 *screw thread*—a helical groove on a cylindrical or conical surface. The projecting helical ridge thus formed is called a screw thread, consisting of peaks (crests) and valleys (roots).

3.1.20 *self-tapping force (N)*—the amount of axial force required to engage the self-tapping features of self-tapping style screws when tested in accordance with [Annex A4](#).

3.1.21 *self-tapping screw*—a screw that has any number of flutes at its tip which are intended to cut the screw's thread form into the bone upon insertion.

3.1.22 *size*—an identification of a screw based on its nominal thread diameter, as defined in Section 6.

3.1.23 *solid core*—a screw that does not contain a cannulation along its longitudinal axis.

3.1.24 *thread diameter*—the largest diameter of the threaded portion of the screw measured over the thread crests. This is also known as the major diameter.

3.1.25 *thread length*—the length of the threaded portion of the screw, measured from the thread runout to the screw tip.

3.1.26 *thread runout*—the intersection of the screw thread with either the screw shaft or screw head.

3.1.27 *torsional yield strength (N-m)*—the point at which the screw reaches its proportional limit when tested in accordance with [Annex A1](#). This will be determined by the offset method. A 2° offset value shall be used.

## 4. Classification

4.1 There are a large variety of medical bone screws currently in use. They may be classified by the definitions provided in Section 3. This specification currently includes information that defines the following types of screws:

4.1.1 *Type HA*—Spherical undersurface of head, shallow, asymmetrical buttress thread, and deep screw head.

4.1.2 *Type HB*—Spherical undersurface of head, deep, asymmetrical buttress thread, and shallow screw head.

4.1.3 *Type HC*—Conical undersurface of head, symmetrical thread.

4.1.4 *Type HD*—Conical undersurface of head, asymmetrical thread.

## 5. Material

5.1 Screws shall be fabricated from a metallic material intended for surgical implant applications, and having ASTM medical material. In addition, the materials shall be biocompatible for the intended application.

## 6. Dimensions and Tolerances

6.1 There are many types of metallic bone screw designs available, so a complete list of dimensions and tolerances for all screws covered by this specification is unfeasible. However, this specification does provide required dimensions and tolerances for four types of screws as classified in 4.1. Screws conforming to this specification, and designated HA, HB, HC, or HD screws, shall be fabricated in accordance with the dimensions and tolerances described in [Annex A5](#) and [Annex A6](#), respectively.

## 7. Finish and Marking

7.1 The screw shall be free from nicks, dents, burrs, and scratches when examined in accordance with Practice [F86](#).

7.2 When size permits, the following information should be legibly marked on the head of the screw (in order of preference):

7.2.1 Manufacturer's name or logo,

7.2.2 *Screw Size*—If a screw is manufactured in accordance with ASTM or ISO specifications, the ASTM or ISO designation should be provided,

7.2.3 Material,

7.2.4 Catalog number, and

7.2.5 Manufacturing lot number.

7.3 Screws shall be marked in accordance with Practice [F983](#), unless otherwise specified in 7.2, in a manner such that the mechanical integrity of the screw is not compromised.

## 8. Care and Handling

8.1 Screws should be cared for and handled in accordance with Practice [F565](#), as appropriate.

## 9. Driving Instruments

9.1 A variety of screwdrivers exist for the insertion and removal of bone screws. The classification and dimensions for various screw-drive recesses currently used in the medical industry are documented in [Annex A7](#). Specification [F116](#) provides related dimensional information for several types of medical screwdrivers.

9.2 Screws conforming to this specification, and designated HA, HB, HC, or HD screws, shall be manufactured with drive recesses that conform to the requirements specified in [Annex A5](#) and [Annex A6](#), respectively.

## 10. Performance Considerations and Test Methods

10.1 The following properties may be important when determining the suitability of a screw for a particular application. However, the test methods referenced as follows may not be appropriate for all types of implant applications. The user is cautioned to consider the appropriateness of the test methods in view of the devices being tested and their potential application.

10.1.1 *Torsional Strength*—This test method is an important parameter to prevent screw breakage during insertion or removal. The torsional strength shall be determined using the test methods described in Annex A1.

10.1.2 *Breaking Angle*—This test method provides a measure of the ductility of the screw when undergoing a torsional moment. A screw with a greater breaking angle may provide an earlier tactile warning to the surgeon that the screw is reaching its maximum torsional strength. The breaking angle shall be determined using the test methods described in Annex A1.

10.1.3 *Axial Pullout Strength*—This test method may be an important parameter if the screw is subjected to axial tensile forces, or if the screw is fixed into poor quality or osteoporotic bone. The pullout strength may be determined using the test methods described in Annex A3.

10.1.4 *Insertion Torque*—This test method may be an important parameter to avoid failure of the screw during insertion and to ensure that the screw may be easily inserted by the surgeon. The insertion torque should be much less than torsional yield strength of the screw and of the appropriate screwdriver bit. The insertion torque may be determined using the test methods described in Annex A2.

10.1.5 *Removal Torque*—This test method may be an important parameter to avoid failure of the screw during removal and to ensure that the screw may be easily removed by the surgeon. The removal torque should be much less than torsional yield strength of the screw and of the appropriate screwdriver bit. The removal torque may be determined using the test methods described in Annex A2.

10.1.6 *Self-Tapping Force*—This test method may be an important parameter to ensure that the screw may be easily inserted by the surgeon, particularly if the screw is fixed in poor quality or osteoporotic bone. The self-tapping force may be determined using the test method described in Annex A4.

## 11. Performance Requirements

11.1 Screws shall meet the mechanical performance requirements specified in its associated specification annex.

## 12. Keywords

12.1 bone screw; dimensions; insertion; performance requirements; pullout; static; test methods; torsion

# iTeh Standards

## ANNEXES

(Mandatory Information)

### A1. TEST METHOD FOR DETERMINING THE TORSIONAL PROPERTIES OF METALLIC BONE SCREWS

#### A1.1. Significance and Use

A1.1.1 This test method is used to measure the torsional yield strength, maximum torque, and breaking angle of the bone screw under standard conditions. The results obtained in this test method are not intended to predict the torque encountered while inserting or removing a bone screw in human or animal bone. This test method is intended only to measure the uniformity of the product tested or to compare the mechanical properties of different, yet similarly sized, products.

#### A1.2. Apparatus

A1.2.1 *Testing Fixture*—The torsion testing apparatus that is to be used for applying the required torque to the specimen shall be calibrated for the range of torques and rotational displacements used in the determination.<sup>5</sup> A suitable testing fixture for the torsional yield strength-maximum torque-breaking angle test is illustrated in Fig. A1.1.

A1.2.1.1 *Test Speed*—The torsional force shall be applied at a constant rate of 1 to 5 r/min.

A1.2.1.2 *Torque Transducer*—A transducer to translate the applied torque into an electrical signal amenable to continuous recording, calibrated over the range of torques, both in the

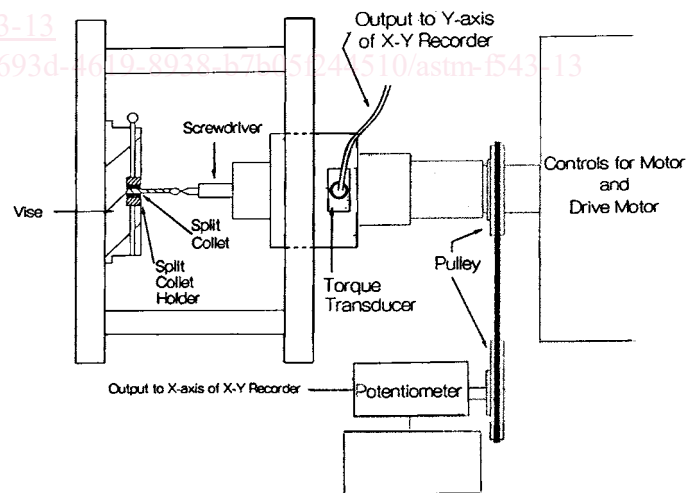


FIG. A1.1 Test Apparatus for Determination of Torsional Breaking Force and Breaking Angle

clockwise and counterclockwise rotation, to be encountered in the test method, shall be provided.

A1.2.1.3 *Torsional Displacement Transducer*—A transducer to translate the angle of twist into an electrical signal amenable to continuous recording, calibrated over the range of angles to

<sup>5</sup> At the time that this specification was approved, no standard test method for the verification of torsion machines or transducers has been accepted. The user is urged to review Terminology E6 and Test Methods E8 for general guidance.



be encountered in the test and an accuracy of  $\pm 0.3^\circ$ , both in the clockwise and counterclockwise rotation, shall be provided.

**A1.2.1.4 Specimen Holder**—A mechanical device to clamp onto the bone screw to prevent its rotation while being stressed without significantly damaging its mechanical integrity shall be provided. One such method is to insert a threaded stopper into the opposite side of a test block. The test block for this holding mechanism will accommodate the insertion of a threaded stopper on the other side of the test block. The threaded stopper will prevent the screw from being completely inserted into the test block and will allow the torsional strength of the screw to be measured. This holder will be modified according to the size of the testing specimen so that the gage length of the specimen will be as outlined in **A1.3.1**.

**A1.2.1.5 Recorder**—The data recorder shall be suitable to continuously record torque versus angle of rotation, calibrated in units of Newton-metres for torque and degrees for angle of rotation. The value of torque shall have a resolution of 5 % of torsional yield strength. The angular displacement scale shall have a minimum sensitivity so as to enable an accurate offset measurement capability for a  $2^\circ$  angular displacement (see **A1.3.3**).

**A1.2.2 Test Specimen**—The test specimen shall be a completely fabricated and finished bone screw.

### A1.3. Procedure

**A1.3.1 Torsional Yield Strength, Maximum Torque, and Breaking Angle**—Place the specimen in the holding device so that five threads, below the head of the screw, are exposed outside the holding device (for example, split collet, and so forth). If the test specimen cannot accommodate this setup because the screw is too small or is partially threaded, alternate procedures may be used. For fully threaded screws that are too small, the gage length of the specimen should represent 20 % of the threaded portion of the test specimen. For partially threaded screws, a large enough portion of the screw thread should be gripped to firmly secure the screw so that it does not rotate when under torsional load. There are no specific requirements on the gage length or the grip length in this case; however, at least one full thread shall be exposed, if possible. Since the gage length and grip length can vary for these screws, the only requirement is that both be reported.

**A1.3.2** The gage length or grip length should be kept the same length for test screws of similar design. If a split collet and collet holder are used, the following test method is appropriate. Place the split collet in the collet holder. Clamp the split collet and holder in the vise. The clamping force of the vise should be sufficient to prevent rotation of the screw or the split collet. Drive the specimen in the direction of insertion, using an appropriate size and configured screwdriver bit, by applying a torsional force. If an axial load is required to maintain the screwdriver bit in the screw head, its value should be noted. The torque wrench shall be driven at a rate of 1 to 5 revolutions/min ( $\tau/\text{min}$ ).

**NOTE A1.1**—The simultaneous use of two chart recorders may simplify the ability to measure torsional yield strength accurately by the offset method. One chart recorder with an angular displacement scale or sensitivity of  $50^\circ/\text{cm}$  is convenient for measuring maximum torque and

breaking angle. A second chart recorder with an angular displacement scale or sensitivity of  $10^\circ/\text{cm}$  or less is suggested to provide accurate offset measurement capability for measuring a  $2^\circ$  angular displacement. Alternatively, one chart recorder and a digital storage oscilloscope may be used.

**A1.3.3** The torsional yield strength will be determined by the offset method (**Fig. A1.2**), using the torque versus angle of rotation curve produced in **A1.3.1** and **A1.3.2**.

**A1.3.3.1** On the torque versus angle of rotation curve, locate Point *m* equal to a rotation of  $2^\circ$ . Draw *mn* parallel to *OA*, and locate *b*, the intersection of *mn* with the torque versus angle of rotation curve. Torque *B* is defined as the torsional yield strength.

**A1.3.3.2** The maximum torque is determined by the largest value of torque on the torque versus angle of rotation curve.

**A1.3.3.3** The breaking angle is determined from the torque versus angle plot shown in **Fig. A1.3**. The breaking angle is defined as the point at which the torque portion of the curve demonstrates its most rapid descent (negative slope) to total failure. The breaking angle (B.A.) is determined as the intersection of the two tangents (*D* and *E*) shown in **Fig. A1.3**. Line *E* is a tangent to the horizontal portion of the curve which represents maximum torque. Line *D* is drawn at the curve's most rapid descent. The intersection of these two lines is the breaking angle (B.A.) and is recorded to the nearest  $10^\circ$ .

### A1.4. Report

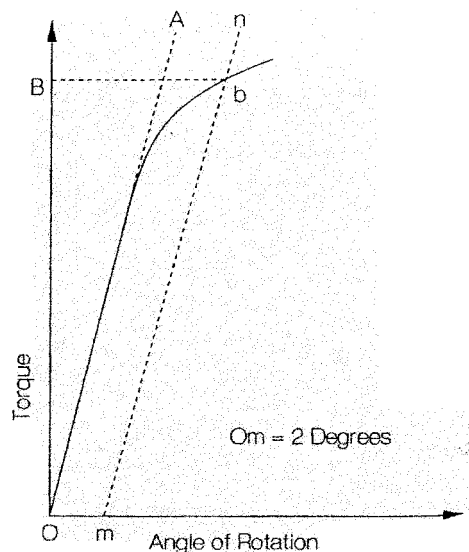
**A1.4.1** Report the following information for each specimen tested:

**A1.4.1.1 Screw Identification**—Reference any applicable ASTM or ISO specification that may apply to the specimen. If specifications do not exist, provide head form, thread form, major and minor diameter, thread pitch, overall screw length, head and shank (unthreaded portion of the screw excluding the head) length, and type of screw point.

**A1.4.1.2** Screw chemical composition. F543-13

**A1.4.1.3** Surface finish.

**A1.4.1.4** Gage length.



**FIG. A1.2 Typical Torque Versus Angle of Rotation Curve**

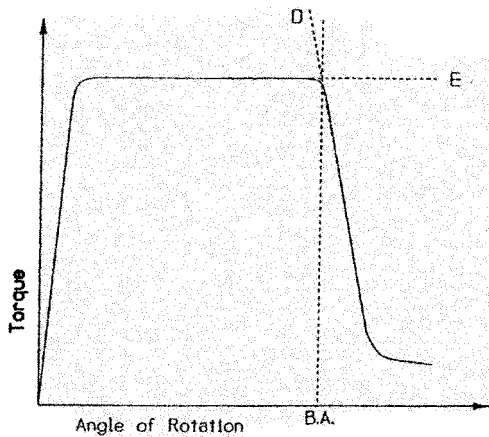


FIG. A1.3 Typical Plot of Torque Versus Torsion Angle

A1.4.1.5 Torsional yield strength.

A1.4.1.6 Maximum torque.

A1.4.1.7 Breaking angle.

A1.4.1.8 Torque versus angle of rotation plot.

A1.4.1.9 The size of the exposed portion of the screwdriver (that is, the length and diameter relative to the tested screw) or the angular deformation of the screwdriver assembly at maximum torque.

A1.4.1.10 *Grip Length*—Does not have to be reported for a fully threaded screw of ASTM or ISO specification whose overall length is given.

A1.4.1.11 *Fracture Location*—The location can be specified by listing the number of threads below the head at which the screw fails or by measuring the distance below the head to the approximate fracture point.

**A1.5. Precision and Bias**

A1.5.1 Data establishing the precision and bias to be expected from this test method have not yet been obtained.

**A2. TEST METHOD FOR DRIVING TORQUE OF MEDICAL BONE SCREWS**

**A2.1. Significance and Use**

A2.1.1 This test method is used to measure the torque required to drive a bone screw into a standard material. The results obtained in this test method bear no direct correlation to the insertion torque required to insert the subject bone screw in human or animal bone. This test method is used only for the purpose of maintaining the uniformity of the product tested.

**A2.2. Apparatus**

A2.2.1 *Testing Fixture*—A suitable test fixture as shown in Fig. A2.1 may be used for the insertion-removal torque tests.<sup>5</sup> This fixture shall incorporate the test block material that conforms to Specification F1839, test block clamp, drill

bushing, and bushing support depicted. It shall be sufficiently rigid to not deflect or deform under the conditions of loading encountered during the test.

A2.2.1.1 *Torque Transducer*—A transducer to translate the applied torque into an electrical signal amenable to continuous recording, calibrated over the range of torques, both in the clockwise and counterclockwise rotation, to be encountered in the test shall be provided.

A2.2.1.2 *Torsional Displacement Transducer*—A transducer to translate the angle of twist into an electrical signal amenable to continuous recording, calibrated in a manner similar to Practices E4 over the range of angles to be encountered in the

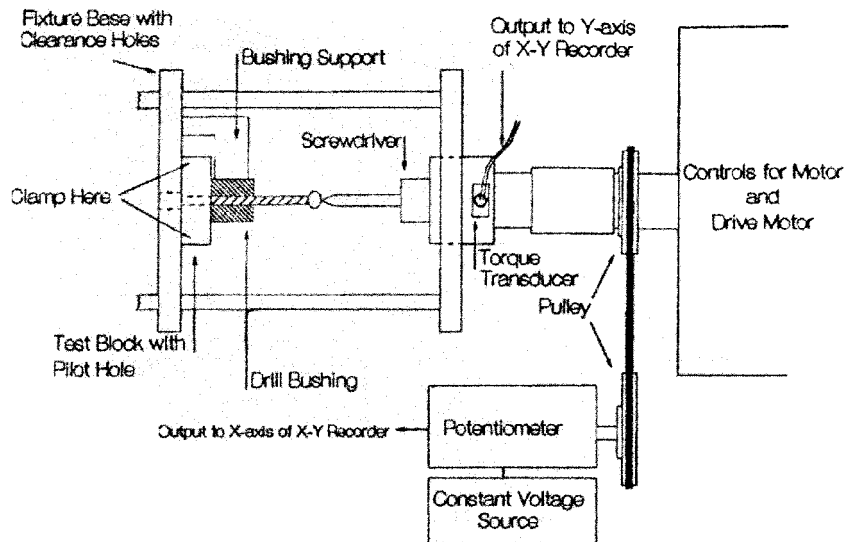


FIG. A2.1 Schematic of Test Apparatus for Driving Force