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**Extracorporeal systems for blood purification — ~~1~~ 2**

**Part 1:  
Haemodialysers, haemodiafilters, haemofilters and  
haemoconcentrators**

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*Systèmes extracorporels pour la purification du sang —*

*Partie 1: Hémodialyseurs, hémodiafiltres, hémofiltres et hémococoncentrateurs*

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### Foreword

ISO (the International Organization for Standardization) is a worldwide federation of national standards bodies (ISO member bodies). The work of preparing International Standards is normally carried out through ISO technical committees. Each member body interested in a subject for which a technical committee has been established has the right to be represented on that committee. International organizations, governmental and non-governmental, in liaison with ISO, also take part in the work. ISO collaborates closely with the International Electrotechnical Commission (IEC) on all matters of electrotechnical standardization.

The procedures used to develop this document and those intended for its further maintenance are described in the ISO/IEC Directives, Part 1. In particular, the different approval criteria needed for the different types of ISO document should be noted. This document was drafted in accordance with the editorial rules of the ISO/IEC Directives, Part 2 (see [www.iso.org/directives](http://www.iso.org/directives)).

ISO draws attention to the possibility that the implementation of this document may involve the use of (a) patent(s). ISO takes no position concerning the evidence, validity or applicability of any claimed patent rights in respect thereof. As of the date of publication of this document, ISO had not received notice of (a) patent(s) which may be required to implement this document. However, implementers are cautioned that this may not represent the latest information, which may be obtained from the patent database available at [www.iso.org/patents](http://www.iso.org/patents). ISO shall not be held responsible for identifying any or all such patent rights.

Any trade name used in this document is information given for the convenience of users and does not constitute an endorsement.

For an explanation of the voluntary nature of standards, the meaning of ISO specific terms and expressions related to conformity assessment, as well as information about ISO's adherence to the World Trade Organization (WTO) principles in the Technical Barriers to Trade (TBT), see [www.iso.org/iso/foreword.html](http://www.iso.org/iso/foreword.html).

This document was prepared by Technical committee ISO/TC 150, *Implants for surgery*, Subcommittee SC 2, *Cardiovascular implants and extracorporeal systems*.

This second edition of ~~ISO 8637-1:2023~~ ~~replaces~~ ~~and~~ replaces the first version of this document (ISO 8637-1:2017), which has been technically revised.

The main changes are as follows:

- ~~Alignment of~~ terms and definitions ~~have been aligned~~ with those defined in ~~other parts of the ISO and IEC databases~~ ~~8637 series~~;
- ~~All Figures have been redrawn, and~~ additional figures relating to gauges used to test dimensional compliance ~~have been~~ added;
- ~~test methods have been revised and an example of a test method for endotoxin transfer measurement~~ ~~has been~~ added;
- ~~requirements for accompanying documentation have been revised.~~

A list of all parts in the ISO 8637 series can be found on the ISO website.

Any feedback or questions on this document should be directed to the user's national standards body. A complete listing of these bodies can be found at [www.iso.org/members.html](http://www.iso.org/members.html).

## ISO/FDIS 8637-1:2024(en)

### Introduction

This document is concerned with devices intended for haemodialysis, haemodiafiltration, haemofiltration and haemoconcentration in humans. If such a device is used with an extracorporeal circuit, the dimensions of the blood ports and filtrate ports have been specified to ensure compatibility of the device with the extracorporeal blood circuit specified in ISO 8637-2. The design and dimensions have been selected to minimize the risk of leakage of blood and the ingress of air.

The requirements specified in this document will help to ensure safety and satisfactory function.

It was not found practicable to specify materials of construction. This document therefore requires only that materials which have been used have been tested and that the methods and results are made available upon request.

There is no intention to specify, or to set limits on, the performance characteristics of the devices because such restrictions are unnecessary for the qualified user and would limit the alternatives available when choosing a device for a specific application. The performance characteristics together with their methods of measurement have been revised and updated to take into consideration developments in technology that have occurred since the ~~previous revision and~~ publication of [the previous edition of this standard document](#).

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# Extracorporeal systems for blood purification ~~—~~ —

## Part 1: Haemodialysers, haemodiafilters, haemofilters and haemoconcentrators

### 1 Scope

This document specifies requirements and test methods for haemodialysers, haemodiafilters, haemofilters and haemoconcentrators, hereinafter collectively referred to as “the device”, for use in humans.

This document does not apply to:

- ~~—~~extracorporeal blood circuits;
- ~~—~~plasmafilters;
- ~~—~~haemoperfusion devices;
- ~~—~~vascular access devices;
- ~~—~~blood pumps;
- ~~—~~systems to prepare, maintain or monitor dialysis fluid;
- ~~—~~systems or equipment intended to perform haemodialysis, haemodiafiltration, haemofiltration or haemoconcentration;
- ~~—~~reprocessing procedures and equipment.

NOTE 1 Requirements for the extracorporeal blood circuit for haemodialysers, haemodiafilters and haemofilters are specified in ISO 8637-2.

NOTE 2 Requirements for plasmafilters are specified in ISO 8637-3.

### 2 Normative references

The following documents are referred to in the text in such a way that some or all of their content constitutes requirements of this document. For dated references, only the edition cited applies. For undated references, the latest edition of the referenced document (including any amendments) applies.

~~ISO 7000, Graphical symbols for use on equipment — Registered symbols~~

ISO 10993-1, *Biological evaluation of medical devices — Part 1: Evaluation and testing within a risk management process*

ISO 10993-4, *Biological evaluation of medical devices — Part 4: Selection of tests for interactions with blood*

ISO 10993-7, *Biological evaluation of medical devices — Part 7: Ethylene oxide sterilization residuals*

ISO 10993-11, *Biological evaluation of medical devices — Part 11: Tests for systemic toxicity*

ISO 11737-2, *Sterilization of health care products — Microbiological methods — Part 2: Tests of sterility performed in the definition, validation and maintenance of a sterilization process*

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~~ISO 11607-1, Packaging for terminally sterilized medical devices — Part 1: Requirements for materials, sterile barrier systems and packaging systems~~

~~ISO 11607-2, Packaging for terminally sterilized medical devices — Part 2: Validation requirements for forming, sealing and assembly processes~~

ISO 14971, Medical devices — Application of risk management to medical devices

~~ISO 15223-1, Medical devices — Symbols to be used with information to be supplied by the manufacturer — Part 1: General requirements~~

~~ISO 15223-2, Medical devices — Symbols to be used with medical device labels, labelling, and information to be supplied — Part 2: Symbol development, selection and validation~~

ISO 17664-1, Processing of health care products — Information to be provided by the medical device manufacturer for the processing of medical devices — Part 1: Critical and semi-critical medical devices

~~ISO 23500-5, Preparation and quality management of fluids for haemodialysis and related therapies — Part 5: Quality of dialysis fluid for haemodialysis and related therapies"~~

~~ISO 20417, Medical devices — Information to be supplied by the manufacturer~~

ISO 80369-7:2021, Small-bore connectors for liquids and gases in healthcare applications — Part 7: Connectors for intravascular or hypodermic applications

~~ISO 90369-20, Small bore connectors for liquids and gases in healthcare applications — Part 20: Common test methods~~

~~ISO 20417, Medical devices — Information to be supplied by the manufacturer~~

### 3 Terms and definitions

For the purposes of this document, the following terms and definitions apply.

ISO and IEC maintain terminology databases for use in standardization at the following addresses: <https://www.iso.org/obp> and <https://www.electropedia.org/>

— ~~ISO Online browsing platform: available at <https://www.iso.org/obp>~~

— ~~IEC Electropedia: available at <https://www.electropedia.org/>~~

#### 3.1

##### **blood compartment**

part of a haemodialyser (3.16(3.14)), haemodiafilter (3.14(3.12)), haemofilter (3.18(3.16)) or haemoconcentrator (3.13(3.11)) through which blood is intended to pass

#### 3.2

##### **blood compartment volume**

volume which is needed to fill the blood compartment

Note 1 to entry: For hollow fibre devices, the blood compartment volume includes the volume of the hollow fibres plus the headers.

#### 3.3

##### **blood compartment connector**

##### **blood connector**

cone type connector to permit the entry and exit of blood and to connect the device to blood tubing sets



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Note 1 to entry: Historically the term blood port was used.

### 3.34

#### clearance

volume of a solution from which a solute is completely removed per unit time

### 3.45

#### convection

transport of a solvent across a semipermeable membrane resulting from a pressure differential across the membrane.

Note 1 to entry: Convective solute transport supplements diffusive transport as a result of "solute drag" whereby solutes contained in the solvent are co-transported with the solvent.

### 3.56

#### convective therapy

forms of renal replacement therapies removing therapy that removes uremic toxins from blood either by convection solely or by a combination of diffusion and convection through a semi permeable membrane.

Note 1 to entry: Convective therapies remove toxins from the blood by removing fluid from the device in excess of that required to achieve the patient's target fluid balance, thereby requiring infusion of replacement fluid into the patient's blood. In contrast, haemodialysis removes fluid from the device only to correct the patient's fluid weight gain realized between dialysis treatments.

Note 2 to entry: Haemofiltration, and haemodiafiltration are types of convective therapies.

Note 3 to entry: Haemoconcentrators are fluid removal devices used during cardiac surgery.

### 3.67

#### dialysis fluid

aqueous fluid containing electrolytes and, usually, buffer and glucose, which is intended to exchange solutes with blood during haemodialysis (3.17(3.15)) or haemodiafiltration (3.15(3.13)).

Note 1 to entry: The term "dialysis fluid" is used throughout this document to mean the fluid (made from dialysis water and concentrates) which is delivered to the haemodialyser or haemodiafilter by a dialysis fluid delivery system. Phrases such as "dialysate", "dialysis solution" or "dialysing fluid" can be used in place of dialysis fluid.

Note 2 to entry: The dialysis fluid entering the haemodialyser or haemodiafilter is referred to as "fresh dialysis fluid", while the fluid leaving the haemodialyser or haemodiafilter is referred to as "spent dialysis fluid" or "effluent".

Note 3 to entry: Dialysis fluid does not include pre-packaged fluids used in some renal replacement therapies.

### 3.78

#### dialysis fluid compartment

part of a haemodialyser (3.16(3.14)) or haemodiafilter (3.14(3.12)) through which dialysis fluid (3.7(3.6)) is intended to pass

### 3.9

#### dialysis fluid connector

dialysate connector

connector forming part of the device to permit the passage of dialysis fluid through the device and to link the device to equipment producing the dialysis fluid

### 3.10

#### diffusion

transport of solutes across a semipermeable membrane, caused by a concentration gradient

**3.911**

**filtrate**

fluid removed from the blood across the semipermeable membrane ~~into the dialysis fluid or filtrate compartment of~~ contained in a haemodialyser (3.16(3.14)), haemodiafilter (3.14(3.12)), haemofilter (3.18(3.16)) or haemoconcentrator (3.13(3.11)), due to a pressure gradient (including the contributions of both hydrostatic and oncotic pressures) across the semipermeable membrane

Note 1 to entry: In a haemodialyser and haemodiafilter, the fluid removed is mixed with dialysis fluid flowing through the device.

**3.1012**

**haemoconcentration**

convective process with the purpose of removing excess plasma water from the patient's blood volume, that has been expanded by physiologic fluid, as typically required during cardiac surgery

**3.1113**

**haemoconcentrator**

device intended to perform haemoconcentration (3.12(3.10))

**3.1214**

**haemodiafilter**

device intended to perform haemodiafiltration (3.15(3.13))

**3.1315**

**haemodiafiltration**

**HDF**

process whereby concentrations of water-soluble substances in a patient's blood and an excess of fluid of a patient are corrected by a simultaneous combination of haemodialysis (3.17) and ultrafiltration (3.23 ~~HD and HF~~)

[SOURCE: IEC 60601-2-16:2018, 201.3.208]

Note 1 to entry: Diffusive solute removal is achieved using a dialysis fluid stream as in haemodialysis. Enhanced convective solute removal is achieved by adding ultrafiltration in excess of that needed to achieve the desired weight loss; fluid balance is maintained by the infusion of a replacement solution into the blood circuit either before (predilution haemodiafiltration) or after (post-dilution haemodiafiltration) or a combination of the two (mixed dilution haemodiafiltration).

**3.14**

[SOURCE: IEC 60601-2-16:2018, 201.3.208, modified — Note 1 to entry has been added.]

**3.16**

**haemodialyser**

device intended to perform haemodialysis (3.17(3.15))

**3.1517**

**haemodialysis**

**HD**

process whereby concentrations of water-soluble substances in a patient's blood and an excess of fluid of a patient are corrected by bidirectional diffusive transport and ultrafiltration across a semi-permeable membrane separating the blood from the dialysis fluid

Note 1 to entry: This process typically includes fluid removal by filtration. This process is usually also accompanied by diffusion of substances from the dialysis fluid into the blood.

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[SOURCE: IEC 60601-2-16:2018, 201.3.209]

**3.1618**  
**haemofilter**

device intended to perform *haemofiltration* (3.19(3.17))

**3.1719**  
**haemofiltration**

**HF**

process whereby concentrations of water-soluble substances in a patient's blood and an excess of fluid of a patient are corrected by convective transport via ultrafiltration and partial replacement by a substitution fluid resulting in the required net fluid removal

[SOURCE: IEC 60601-2-16:2018, 201.3.211]

Note 1 to entry: In haemofiltration, there is no dialysis fluid stream.

**3.1820**  
**labelling**

written, printed, graphic or electronic matter that is affixed to a device (haemodialyser, haemodiafilter, haemofilter or haemoconcentrator) or any of its containers or wrappers, or accompanies a device and which is related to identification, technical description and use of that device, but excluding shipping documents

**3.1921**  
**sieving coefficient**

ratio of a solute concentration in the filtrate to the simultaneous concentration of the same solute in the plasma

**3.2022**  
**transmembrane pressure**  
**TMP**

$p_{TM}$

mean pressure exerted across a semipermeable membrane

Note 1 to entry: For practical reasons, the mean TMP is generally expressed as either:

— the difference between arithmetic means of inlet and outlet pressures of the blood and dialysis fluid compartments of a haemodialyser or a haemodiafilter; or

~~or~~

— the difference between the arithmetic mean of the inlet and outlet pressures of the blood compartment and the filtrate pressure of a haemofilter or a haemoconcentrator.

**3.2123**  
**ultrafiltration**  
**UF**

pressure driven process employing a hydraulic pressure gradient applied to a semipermeable membrane

Note 1 to entry: In haemodialysis treatment ultrafiltration generally refers to the removal process used to remove excess fluid from the patient

**3.2224**  
**ultrafiltration coefficient**

permeability of the device to plasma water;

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Note 1 to entry: The ultrafiltration coefficient is generally expressed in ~~milliliters~~ millilitres per hour per millimetre of mercury.

### ~~3.23~~ 3.25

#### ultrafiltration rate

#### UFR

filtrate flow rate from the blood compartment to the dialysis fluid compartment caused by a pressure gradient or pressure differential across the membrane measured as volume per time

Note 1 to entry: Ultrafiltration rate is expressed in ml/min or l/h.

## 4 Requirements

### 4.1 Biological safety and haemocompatibility

Parts of the device that are intended to come into direct or indirect contact with blood shall be evaluated for freedom from biological hazards, in accordance with 5.25.2. If the device is labelled for reuse, testing shall be performed after reprocessing following the manufacturer's instructions for use.

Attention is drawn to the need to establish whether national regulations or national standards governing toxicology and biocompatibility testing exist in the country in which the device is produced and, if applicable, in the countries in which the device is to be marketed.

### 4.2 Sterility

The blood pathway of the device shall be sterile and the state of sterility of the device shall comply with the manufacturer's statement [see 7.2(7.2, h)- h].

Compliance shall be verified in accordance with 5.35.3.

### 4.3 Non-pyrogenicity

The blood pathway of the device shall be non-pyrogenic and the state of non-pyrogenicity of the device shall comply with the manufacturer's statement [see 7.2(7.2, h)- h].

Compliance shall be verified in accordance with 5.45.4.

### 4.4 Mechanical characteristics

#### 4.4.1 Structural integrity

The device external casing shall be capable of withstanding a positive pressure of 1,5 times of the manufacturer's recommended maximum pressure above atmospheric pressure and a negative pressure not exceeding 66,7 kPa (500 mmHg) below atmospheric pressure, when tested in accordance with 5.5.1 according to 5.5.1.

#### 4.4.2 Blood compartment integrity

When exposing the blood compartment of the device to a validated test procedure performed at 1,5 times of the manufacturer's maximum recommended transmembrane pressure, the blood compartment shall not leak.

Compliance with this requirement shall be verified in accordance with 5.5.25.5.2.

#### 4.4.3 Haemodialyser, haemodiafilter and haemofilter blood compartment connectors

Except where the device and the extracorporeal blood circuit are designed as an integral system, the dimensions of the blood compartment connectors shall be as given in Figure 1Figure and Table 1.

Compliance with this requirement shall be verified in accordance with 5.5.3.25.5.3.2.