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Standard Specification and Test Methods for Intramedullary Fixation Devices¹

This standard is issued under the fixed designation F1264; the number immediately following the designation indicates the year of original adoption or, in the case of revision, the year of last revision. A number in parentheses indicates the year of last reapproval. A superscript epsilon (ϵ) indicates an editorial change since the last revision or reapproval.

1. Scope

1.1 This specification is intended to provide a characterization of the design and mechanical function of intramedullary fixation devices (IMFDs), specify labeling and material requirements, provide test methods for characterization of IMFD mechanical properties, and identify needs for further development of test methods and performance criteria. The ultimate goal is to develop a standard which defines performance criteria and methods for measurement of performance-related mechanical characteristics of IMFDs and their fixation to bone. It is not the intention of this specification to define levels of performance or case-specific clinical performance of these devices, as insufficient knowledge to predict the consequences of the use of any of these devices in individual patients for specific activities of daily living is available. It is not the intention of this specification to describe or specify specific designs for IMFDs.

1.2 This specification describes IMFDs for surgical fixation of the skeletal system. It provides basic IMFD geometrical definitions, dimensions, classification, and terminology; labeling and material specifications; performance definitions; test methods and characteristics determined to be important to *in-vivo* performance of the device.

1.3 *Multiple test methods are included in this standard. However, the user is not necessarily obligated to test using all of the described methods. Instead, the user should only select, with justification, test methods that are appropriate for a particular device design. This may be only a subset of the herein described test methods.*

1.4 This specification includes four standard test methods:

1.4.1 Static Four-Point Bend Test Method—**Annex A1** and

1.4.2 Static Torsion Test Method—**Annex A2**.

1.4.3 Bending Fatigue Test Method—**Annex A3**.

1.4.4 Test Method for Bending Fatigue of IMFD Locking Screws—**Annex A4**.

1.5 A rationale is given in **Appendix X1**.

1.6 The values stated in SI units are to be regarded as standard. No other units of measurement are included in this standard.

2. Referenced Documents

2.1 *ASTM Standards:*²

A214/A214M Specification for Electric-Resistance-Welded Carbon Steel Heat-Exchanger and Condenser Tubes

A450/A450M Specification for General Requirements for Carbon and Low Alloy Steel Tubes

D790 Test Methods for Flexural Properties of Unreinforced and Reinforced Plastics and Electrical Insulating Materials

E4 Practices for Force Verification of Testing Machines

E691 Practice for Conducting an Interlaboratory Study to Determine the Precision of a Test Method

F86 Practice for Surface Preparation and Marking of Metallic Surgical Implants

F138 Specification for Wrought 18Chromium-14Nickel-2.5Molybdenum Stainless Steel Bar and Wire for Surgical Implants (UNS S31673)

F339 Specification for Cloverleaf Intramedullary Pins (Withdrawn 1998)³

F383 Practice for Static Bend and Torsion Testing of Intramedullary Rods (Withdrawn 1996)³

F565 Practice for Care and Handling of Orthopedic Implants and Instruments

¹ This specification is under the jurisdiction of ASTM Committee F04 on Medical and Surgical Materials and Devices and is the direct responsibility of Subcommittee F04.21 on Osteosynthesis.

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² For referenced ASTM standards, visit the ASTM website, www.astm.org, or contact ASTM Customer Service at service@astm.org. For *Annual Book of ASTM Standards* volume information, refer to the standard's Document Summary page on the ASTM website.

³ The last approved version of this historical standard is referenced on www.astm.org.

[F1611 Specification for Intramedullary Reamers](#)

[F2503 Practice for Marking Medical Devices and Other Items for Safety in the Magnetic Resonance Environment](#)

[F2809 Terminology Relating to Medical and Surgical Materials and Devices](#)

2.2 *AMS Standard:*

[AMS 5050 Steel Tubing, Seamless, 0.15 Carbon, Maximum Annealed](#)⁴

2.3 *SAE Standard:*

[SAE J524 Seamless Low-Carbon Steel Tubing Annealed for Bending and Flaring](#)⁴

3. Terminology

3.1 *Definitions for Geometric:*

3.1.1 *closed section, n*—any cross section perpendicular to the longitudinal axis of a solid or hollow IMFD in which there is no discontinuity of the outer wall.

3.1.1.1 *Discussion*—To orient the IMFD for testing and for insertion, the desired relationship of any irregularities, asymmetries, and so forth, to the sagittal and coronal planes for the intended applications should be described.

3.1.2 *IMFD curvature, n*—dimensions of size and locations of arcs of the curvature, or mathematical description of the curvature, or other quantitative descriptions to which the curvature is manufactured along with tolerances.

3.1.2.1 *Discussion*—To orient the IMFD for testing and for insertion, the desired relationship of the curvature to the sagittal and coronal planes for the intended applications should be described.

3.1.3 *IMFD diameter, n*—diameter of the circumscribed circle that envelops the IMFD's cross section when measured along its working length. If the diameter is not constant along the working length, then the site of measurement should be indicated.

3.1.4 *IMFD length, n*—length of a straight line between the most proximal and distal ends of the IMFD.

3.1.5 *open section, n*—any cross section perpendicular to the longitudinal axis of a hollow IMFD in which there is a discontinuity of the outer wall.

3.1.5.1 *Discussion*—To orient the IMFD for testing and insertion, the desired relationship of the discontinuity to the sagittal and coronal planes for the intended applications should be described.

3.1.6 *potential critical stress concentrator (CSC), n*—any change in section modulus, material property, discontinuity, or other feature of a design expected to cause a concentration of stress in a region of the IMFD expected to be highly stressed under the normal anticipated loading conditions.

3.1.7 *tolerance, n*—acceptable deviations from the nominal size of any dimension describing the IMFD.

3.1.8 *working length, n*—length of uniform cross section of the IMFD intended to obtain some type of fit to the medullary canal in the area of the diaphysis.

3.2 *Definitions—Mechanical/Structural:*

3.2.1 *bending compliance, n*—reciprocal of the stiffness of the IMFD under a bending load in a specified plane as defined and determined in the static four-point bend test described in [Annex A1](#).

3.2.2 *failure strength, n*—the force parameter (for example, load, moment, torque, stress, and so forth) required to meet the failure criteria, as defined and measured according to the test conducted. (See [Note 1](#).)

NOTE 1—No present testing standard exists related to this term for IMFDs.

3.2.3 *fatigue strength at N cycles, n*—the maximum cyclic force parameter (for example, load, moment, torque, stress, and so forth) for a given load ratio, which produces device structural damage or meets some other failure criterion in no less than *N* cycles as defined and measured according to the test conducted.

3.2.4 *N*—a variable representing a specified number of cycles.

3.2.5 *no load motion*—relative motion between the IMFD and the bone that occurs with no elastic strain in the device and no (or minimal) change in load. (See [Note 1](#).)

3.2.6 *structural stiffness, n*—the maximum slope of the elastic portion of the load-displacement curve as defined and measured according to the test conducted.

3.2.6.1 *Discussion*—For bending in a specified plane, this term is defined and determined in the static four-point bend test described in [Annex A1](#).

3.2.7 *ultimate strength, n*—maximum force parameter (for example, load, moment, torque, stress, and so forth) which the structure can support, defined and measured according to the test conducted.

3.2.8 *yield strength, n*—the force parameter (for example, load, moment, torque, stress, and so forth) which initiates permanent deformation as defined and measured according to the test conducted.

4. Classification

4.1 The following IMFDs may be used singly, multiply, and with or without attached supplemental fixation: solid cross section, hollow cross section (open, closed, or a combination).

⁴ Available from Society of Automotive Engineers (SAE), 400 Commonwealth Dr., Warrendale, PA 15096-0001, <http://www.sae.org>.

4.2 Intended application or use for particular IMFD designs:

4.2.1 *Preferred Orientation:*

4.2.1.1 Right versus left,

4.2.1.2 Sagittal versus coronal plane,

4.2.1.3 Proximal versus distal, and

4.2.1.4 Universal or multiple options.

4.2.2 *Preferred Anatomic Location:*

4.2.2.1 Specific bone,

4.2.2.2 Proximal versus distal versus midshaft, and

4.2.2.3 Universal or multiple options.

4.2.3 *Preferred Use Limited to Specific Procedures:*

4.2.3.1 Acute care of fractures,

(a) Specific types,

(1) Specific types,

(2) Specific locations,

(b) Specific locations,

4.2.3.2 Reconstructive procedures, and

4.2.3.3 Universal or multiple options.

5. Material

5.1 All IMFDs made of materials that have an ASTM standard shall meet those requirements given in the ASTM standards (2.1).

6. Performance Considerations and Test Methods

6.1 *Cross Section Dimensional Tolerances* affect matching the bone preparation instruments (that is, reamers) to the IMFD diameter, and the IMFD in the bone.

6.1.1 Terminology related to sizing of IMFD devices and instruments is provided in Specification **F1611**.

6.2 *Longitudinal Contour Tolerances* (along with bending compliance) affect the fit and fixation of IMFDs in the bone.⁴

6.3 *Fatigue Strength* affects the choice of implant in cases in which delayed healing is anticipated (that is, infected nonunions, allografts, segmental loss, multiple trauma, and so forth).

6.3.1 The fatigue strength or fatigue lives or both for IMFDs subjected to cycle bending forces shall be determined using the cyclic bending fatigue test method in **Annex A3**.

6.3.2 The fatigue strength or fatigue lives or both for IMFD locking screws subjected to cyclic bending forces shall be determined using the cyclic bending fatigue test method for locking screws in **Annex A4**.

6.4 *Bending Strength* affects the choice of implant in which load sharing is minimized or loading is severe or both (that is, with distal or proximal locking, subtrochanteric fractures, comminuted fracture, segmental loss, noncompliant patient, and so forth).

6.4.1 Yield, failure, and ultimate strength for IMFDs subjected to bending in a single plane shall be determined using the static four-point bend test method described in **Annex A1**.

6.5 *Bending and Torsional Stiffness* may affect the type and rate of primary or secondary healing, depending upon the fracture type (transverse, oblique, and so forth).

6.5.1 Bending structural stiffness for IMFDs subjected to bending in a single plane shall be determined using the static four-point bend test method described in **Annex A1**.

6.5.2 Torsional stiffness for IMFDs subjected to pure torsion shall be determined using the static torsion test method described in **Annex A2**.

6.6 *No-Load Axial and Torsional Motion Allowed in Devices Using Secondary Attached Fixation* affects degree of motion at the fracture site. (See **Note 1**.)

6.7 *Extraction System*—Mechanical failures should occur in the extraction device before they occur in the IMFD. This prevents the need to remove the IMFD without proper tools. (See **Note 1**.)

7. Marking, Packaging, Labeling, and Handling

7.1 Dimensions of IMFDs should be designated by the standard definitions given in **3.1**.

7.2 IMFDs should be marked using a method in accordance with Practice **F86**.

7.3 Use the markings on the IMFD to identify the manufacturer or distributor. Mark away from the most highly stressed areas where possible.

7.4 Packaging shall be adequate to protect the IMFD during shipment.

7.5 The following shall be included on package labeling for IMFDs:

- 7.5.1 Manufacturer and product name,
- 7.5.2 Catalog number,
- 7.5.3 Lot or serial number,
- 7.5.4 IMFD diameter (3.1.3), and
- 7.5.5 IMFD length (3.1.4).

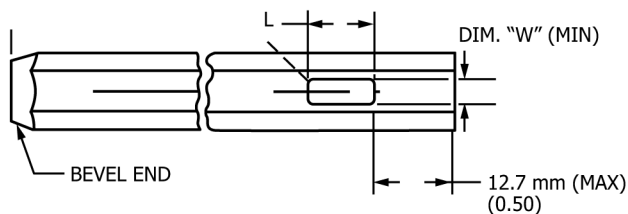
7.6 IMFDs should be cared for and handled in accordance with Practice F565.

7.7 Consider Practice F2503 to identify potential hazards produced by interactions between the device and the MR environment and for terms that may be used to label the device for safety in the MR environment.

8. Means for Insertion and Extraction

8.1 For IMFDs that are to be extracted using a hook device, the following requirements apply:

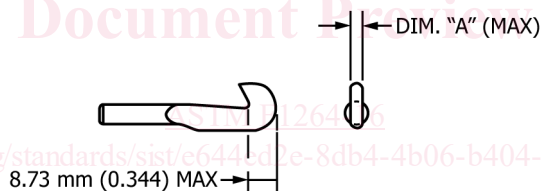
8.1.1 The slot at the end of the IMFD shall have the dimensions shown in Fig. 1.



IMFD Diameter, mm	Hook Size	Slot Length, L, mm	Slot Width, W, mm
6, 7	2	9.53	1.91
8 and larger	1	9.53	3.23

FIG. 1 Dimensions of Extractor Hook Slot

8.1.2 The hook used for extraction shall have the dimensions shown in Fig. 2.



Hook Size	Hook Width, A, mm
1	3.05
2	1.78

FIG. 2 Dimensions of Extractor Hook

9. Keywords

9.1 bend testing; definitions; extraction; fatigue test; fracture fixation; implants; intramedullary fixation devices; orthopaedic medical device; performance; surgical devices; terminology; test methods; torsion test; trauma

ANNEXES**(Mandatory Information)****A1. TEST METHOD FOR STATIC FOUR-POINT BEND TEST****A1.1. Scope**

A1.1.1 This test method describes methods for static four-point bend testing of intrinsic, structural properties of intramedullary fixation devices (IMFDs) for surgical fixation of the skeletal system. This test method includes bend testing in a variety of planes relative to the major anatomic planes. The purpose is to measure bending strength and bending stiffness intrinsic to the design and materials of IMFDs.

A1.1.2 This test method is designed specifically to test IMFD designs that have a well-defined working length (WL) of uniform open or closed cross section throughout the majority of its length ($WL \geq 10 \times$ diameter) and shall be applied to the full length of the diaphysis of a femur, tibia, humerus, radius, or ulna. This is not applicable to IMFDs that are used to fix only a short portion of the diaphysis of any of the long bones or the diaphysis of small bones such as the metacarpals, metatarsals, phalanges, and so forth.

A1.1.3 This test method is not intended to test the extrinsic properties (that is, the interaction of the device with bone or other biologic materials), of any IMFD.

A1.1.4 This test method is not intended to define case-specific clinical performance of these devices, as insufficient knowledge to predict the consequences of the use of any of these devices in individual patients is available.

A1.1.5 This test method is not intended to serve as a quality assurance document, and thus, statistical sampling techniques for batches from production of IMFDs are not addressed.

A1.1.6 This test method may not be appropriate for all types of implant applications. The user is cautioned to consider the appropriateness of the method in view of the devices being tested, the material of their manufacture, and their potential applications.

A1.1.7 This test method is intended to evaluate the bending strength or bending stiffness of the working length of the IMFD, and may not be appropriate for all situations. When the structurally critical region of the IMFD is shown to be located at the proximal or distal extremity of the IMFD, it may be necessary to evaluate the bending strength or bending stiffness of this region of the IMFD using a different test method. This is because it may not be physically possible to fit the proximal or distal extremity between the inner rollers of a four point bend test. Structurally critical regions may be identified through such methods as hand calculations, finite element analysis, etc. Screw holes or other interlocking features are typically located at the proximal and distal extremities of an IMFD, and may result in structurally critical regions at these locations.

A1.1.8 The values stated in SI units are to be regarded as standard. No other units of measurement are included in this standard.

A1.1.9 *This standard does not purport to address all of the safety concerns, if any, associated with its use. It is the responsibility of the user of this standard to establish appropriate safety and health practices and determine the applicability of regulatory limitations prior to use.*

A1.2. Terminology**A1.2.1 Definitions:**

A1.2.1.1 *bending compliance, n* —reciprocal of the stiffness of the IMFD under a bending load in a specified plane ($1/EI_e$ for the IMFD, y/F for the system tested).

A1.2.1.2 *bending moment, n* —moment required to meet predetermined failure criteria.

A1.2.1.2.1 Discussion—

Failure may be defined as permanent deformation, breakage, or buckling.

A1.2.1.3 *bending moment to yield, n* —moment which produces plastic deformation as defined by the 0.2 % strain offset method from the load-displacement curve.

A1.2.1.4 *bending structural stiffness, n* —resistance to bending of an IMFD, normalized to the cross-sectional properties of the working length without regard to the length of IMFD tested, by the calculations described in A1.5.1.8 (the effective EI_e for the region tested).

A1.2.1.5 *fixture/device compliance, n* —measurement of the combined compliance of the IMFD on the test fixture with co-aligned load-support points (such as A1.7.2). This value is dependent upon IMFD orientation, load direction and load and support spans.

A1.2.1.6 *ultimate bending moment, n* —moment at the maximum or ultimate load as measured on the load-displacement curve for any test in accordance with A1.6.1.

A1.2.2 *Definitions of Terms Specific to This Standard:*

A1.2.2.1 The testing mode shall consist of an applied compression load cycle, at a constant displacement rate, to a defined failure.

A1.2.2.2 The testing mode shall be single cycle with the load applied at least three diameters of the IMFD from the nearest critical stress concentration point (CSC) unless otherwise specified or unless the CSC is a characteristic of the normal cross section in the working length.

A1.3 Classification

A1.3.1 *Types of Test Covered by This Specification Are:*

A1.3.1.1 Measurement of structural mechanical behavior inherent to IMFDs—intrinsic properties.

A1.3.1.2 Measurement of single-cycle elastic stiffness and strength in four-point bending.

A1.3.1.3 Measurement of a single-cycle fixture/device elastic compliance.

A1.4. Significance and Use

A1.4.1 This test method describes a static bending test to determine the bending stiffness and bending strength of the central and uniform portions of an IMFD.

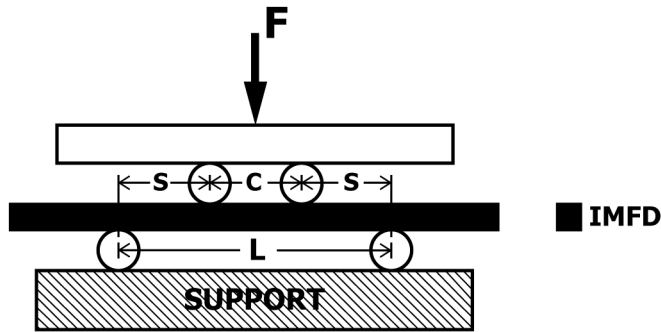
A1.4.2 This test method may not be appropriate for all types of implant applications (i.e., in proximal or distal extremity of an IMFD where screw holes exist). The user is cautioned to consider the appropriateness of the method in view of the devices being tested and their potential applications.

A1.5. Procedure

A1.5.1 *Bending Test for Intrinsic Properties of the Working Length (WL):*

A1.5.1.1 Determine the spans to be used as described in A1.5.1.2 and A1.5.1.3 and set the spans, s , c , and L to within 1 % of the determined values.

A1.5.1.2 Conduct the four-point bending test at room atmospheric conditions as shown in Fig. A1.1, using two rolling supports spaced from 10 to 50 cm apart, L , with the span between the loading points, c , no greater than $L/3$. The loading points should also



RANGE OF SPANS, in mm
L = 100 -> 500
s = 33 -> 250
c = 0 -> 167

FIG. A1.1 Four-Point Bend Test Setup

be of the rolling type, and the diameter of both the loading and support rollers should be between 1.0 and 2.6 cm. The choice of spans should be made based upon the guidelines given in A1.7.2.

A1.5.1.3 A recommendation for load and support spans is provided below to minimize interlaboratory variability and provide consistency with the previous ASTM standard for four-point bend testing of IMFDs. The suggested long or short span should be used whenever possible, provided the general guidelines of A1.7.2 are achieved. The short span is identical to that used in the previous standard, Practice F383, and the long span is based upon the experience of several laboratories testing a broad range of designs and sizes of current (1995) IMFD designs.

Short span
 Long span

s = c = 38 mm
 s = c = 76 mm

L = 114 mm
 L = 228 mm

A1.5.1.4 Apply equal loads at each of the loading points (a single load centered over the load points as shown in Figs. A1.1 and A1.2 is the usual method) at a constant rate of displacement no greater than 1 mm/s. Measure the relative deflections between the support and loading points (inner versus outer), y . For devices made of strain-rate-sensitive materials, the displacement rate for a given strain rate may be estimated by using the following approximations:

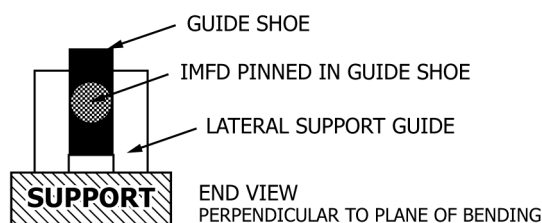
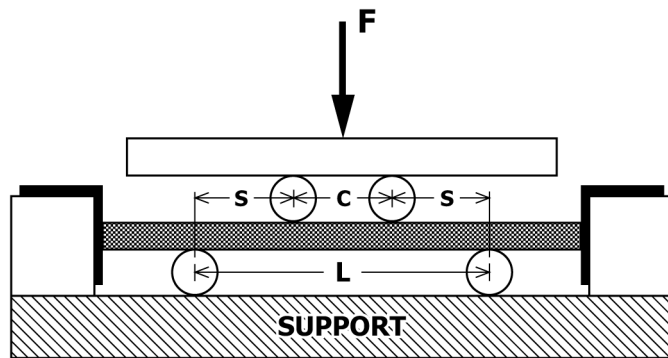


FIG. A1.2 Four-Point Bend Test with Guide Shoes

$$y_{1\%} = S_{t\ 1\%}, \text{ and } c = L - 2s \quad (\text{A1.1})$$

$$y_{1\%} = s(L+2c)/(300 D_{IMFD}) \quad (\text{A1.2})$$

$$= s(3L - 4s)/(300 D_{IMFD})$$

or

$$= s(3c + 2s)/(300 D_{IMFD})$$

where:

- S_t = the desired strain rate,
- $y_{1\%}$ = the deflection at the loading point for an estimated 1 % maximum strain in the IMFD,
- s = the span from a load point to the nearest support,
- c = the center span,
- L = the total span ($c + 2s$), and
- D_{IMFD} = the diameter of the IMFD.

NOTE A1.1—Deflection rate that corresponds to the desired strain rate is only a rough estimate based upon the assumptions of plane strain for closed-section tubes or solid rods so that the neutral axis of the cross section lies uniformly throughout the working length in the center of the circumscribed circle of the cross section and there is material in the cross section touching the circumscribed circle where it intersects the plane of bending.

A1.5.1.5 Compute the bending moment, M , as used in A1.2.1 as follows:

$$M = Fs/2 \quad (\text{A1.3})$$

where:

- F = the force applied to the system (two times the force applied to each of the loading points) and
- s = the span from a load point to the nearest support.

A1.5.1.6 Compute an estimate for the maximum strain in the IMFD as follows:

$$S_{MAX} = FS D_{IMFD} (4 EI_e)^{-1} \quad (\text{A1.4})$$

$$y = Fs^2 (L+2c) (12 EI_e)^{-1} \quad (\text{A1.5})$$

<https://standards.iteh.ai/catalog/standards/sist/e644ed2e-8db4-4b06-b404-4a733f5c2662/astm-f1264-16>

where:

- S_{MAX} = estimate of maximum strain in the IMFD,
- F = force on the system,
- s = span from a load point to the nearest support point,
- EI_e = effective structural stiffness of the IMFD portion tested,
- D_{IMFD} = diameter of the IMFD,
- L = the total span between supports ($2s + c$), and
- c = the center span.

A1.5.1.7 Compute the bending moment to yield by estimating the load at 0.2 % maximum plastic strain. This can be approximated by calculating as follows:

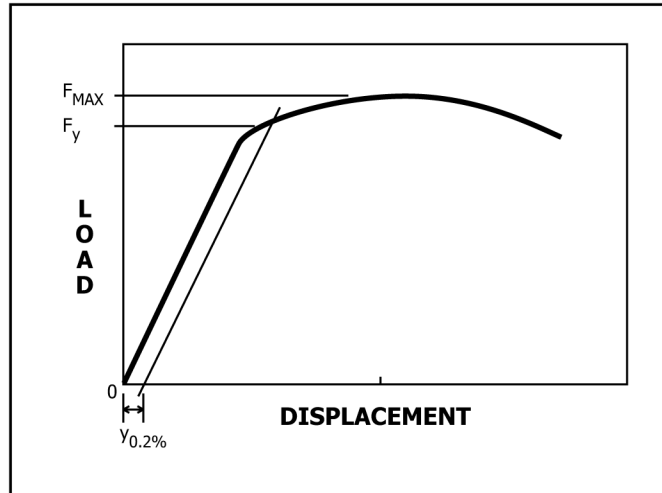
$$y_{0.2\%} = s(L+2c)/(1500 D_{IMFD}) \quad (\text{A1.6})$$

where:

- $y_{0.2\%}$ = the permanent deflection at the loading point for 0.2 % maximum plastic strain (estimated by measuring the offset displacement from the linear region of the load-displacement curve),
- s = the span from a load point to the nearest support,
- c = the center span,
- L = the total span ($c + 2s$), and
- D_{IMFD} = the diameter of the IMFD.

At this point on the load-deflection curve, read the yield force, F_y . From F_y , the bending moment to yield is computed from:

$$M_y = F_y s/2 \text{ (see Fig. A1.3)} \quad (\text{A1.7})$$



NOTE 1—An estimate of a 0.2 % yield point can be made from the “load cell versus ram displacement” measurements. Load represents the total load on the system (2× the load at each support) and the displacement represents the deflection at the load point(s) relative to the supports in the y (or vertical) direction. Setting $S_{MAX} = 0.002$ in the strain estimate equation (A1.5.1.6) and substituting into y gives:

$$y_{0.2\%} = 2 s (L + 2c) (3D_{IMFD})^{-1} \times 10^{-3}$$

where: $y_{0.2\%}$ = an estimate of the deflection at the load point which corresponds to 0.2 % strain.

FIG. A1.3 Load Cell Versus Ram Displacement Graph

Likewise, the ultimate bending moment, M_{MAX} , may be determined from the load-deflection curve as follows:

$$M_{MAX} = F_{MAX}s/2 \text{ (see Fig. A1.3)} \tag{A1.8}$$

NOTE A1.2—The estimate of the deflection that corresponds to the 0.2 % desired strain is only a rough estimate based upon the assumptions of plane strain for closed section tubes or solid rods so that the neutral axis of the cross section lies uniformly throughout the working length in the center of the circumscribed circle of the cross section and that there is material in the cross section touching the circumscribed circle where it intersects the plane of bending.

A1.5.1.8 Compute the bending structural stiffness, EI_e , as follows:

$$EI_e = s^2(L+2c)(F/y)/12 \tag{A1.9}$$

or <https://standards.iteh.ai/catalog/standards/sist/e644ed2e-8db4-4b06-b404-4a733f5c2662/astm-f1264-16>

$$EI_e = s^2(3L - 4s)(F/y)/12 \tag{A1.10}$$

where:

- F/y = the slope of the elastic portion of the load-displacement curve,
- s = the span from a load point to the nearest support,
- c = the center span, and
- L = the total span ($c + 2s$).

NOTE A1.3—If no linear range can be easily approximated from the load-displacement curve, the ratio of the bending load to yield to the total deflection produced by that load at the loading point can be used to estimate the average slope of the elastic range of bending.

A1.5.1.9 Bending should be applied in the planes of maximum (I_{max}) and minimum (I_{min}) area moments of inertia of the working length cross section, and the orientation of the principal inertia axes relative to the medial-lateral (ML) and anterior-posterior (AP) anatomic planes should be reported. If the working length of the IMFD does not have a uniform cross section, or is twisted such that the orientation of the principal inertial axes are not constant along its length, then the IMFD should be loaded to the ML and AP anatomic planes, with the IMFD oriented relative to the anatomic planes as for its intended clinical application.

A1.5.1.10 For IMFDs that have rotational instability for any given bending mode, the ends should be gripped by the fixtures shown in Fig. A1.2. This fixture will allow the IMFD to be constrained outside the actively loaded region by plates that prevent rotation of the IMFD while allowing in-plane bending with supported, free ends in such a manner that the ends are stable when the IMFD rests on the outer support rollers. The use of guide shoes will produce a mixed loading condition as a result of friction in the portion of the system that resists rotation and this will contribute to the bending resistance. The magnitude of this effect is not easily measured or estimated but should be noted in the report.

A1.5.2 *Fixture/Device Compliance Test for the Intrinsic Properties of the Working Length:*

A1.5.2.1 Align both of the supports directly in line with the load points (see Fig. A1.4).

A1.5.2.2 Place the working length of the IMFD between the load point and support. Orient the IMFD so that the load is applied in the desired plane (*AP*, *ML*, or another specified direction).

A1.5.2.3 Load the IMFD in compression at a constant displacement rate of 0.1 mm/s. Record the slope of the load-displacement curve.

A1.5.2.4 Calculate the fixture/device compliance by calculating the reciprocal of the slope of the load-displacement curve in the elastic region and express in mm/N.

A1.6 Number of Specimens

A1.6.1 At least three specimens shall be tested for each sample of IMFD of uniform working length within the test span of the same design, size, material, and so forth tested.

A1.7 Apparatus

A1.7.1 Machines used for the bending tests should conform to the requirements of Practices E4.

A1.7.2 The purpose of allowing a variety of spans and roller diameters for the bending tests is to allow one to accommodate the design differences of devices while maintaining standard techniques. For hollow and open-section IMFDs, long spans and large-diameter rollers will minimize local artifacts at the load and support points as much as possible. For long, small-diameter, solid section IMFDs, much smaller rollers and smaller spans are adequate to measure the bending of the IMFD (see A1.5.1.2).

A1.8. Precision and Bias

A1.8.1 *Minimizing and Correcting for Test Errors:*

A1.8.1.1 Because of differences in cross-sectional shapes, areas, working lengths, and so forth, sensitivity to potential sources of measurement error will be different for each device. Typical sources of error include: (1) span measurements, (2) compliance of the IMFD at the support, (3) fixture compliance, and (4) shear load produced at the load and support points in proportion to bending produced.

A1.8.1.2 *Span Measurement*—In general, longer spans minimize the effect of measurement error. However, the effect of particular measurement errors can be minimized by proper selection of the support and load spans. For example, calculated structural stiffness, EI_c , is more sensitive to errors in measurement of load-to-support point distance, s , than in the center span, c , because

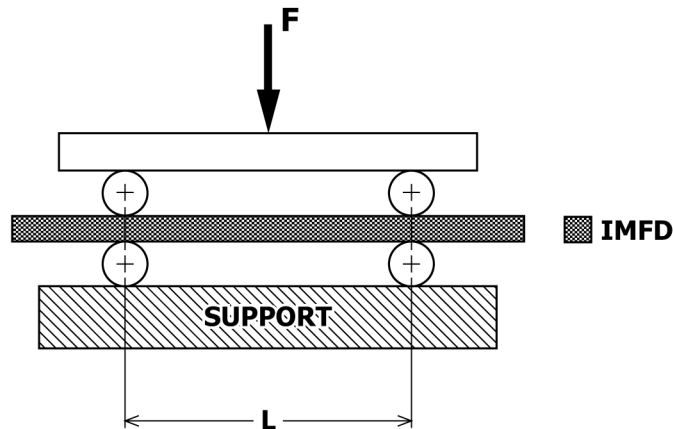


FIG. A1.4 Fixture/Device Compliance Test Setup